

Integration in FACETS

a collaborative software tool-chain for
neuromorphic computation

Andrew Davison
UNIC, CNRS,
Gif sur Yvette,
France

<http://www.andrewdavison.info>

Frontiers in Neuromorphic Computation. Paris. 3-4 June 2010

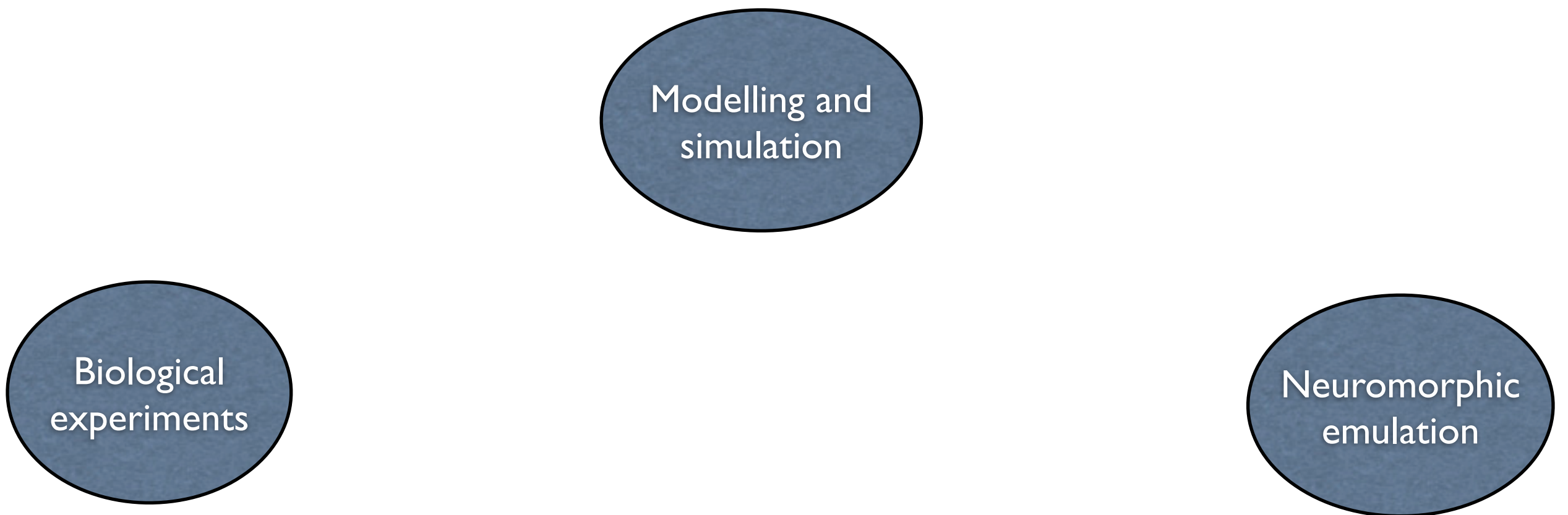


We heard today and yesterday about the range of activities going on in FACETS, from biological experiments, through numerical simulations to neuromorphic hardware development.

Now I'm going to talk about some of the interactions between these different activities.



This presentation is licenced under a Creative Commons Attribution-Noncommercial-Share Alike 3.0 licence
<http://creativecommons.org/licenses/by-nc-sa/3.0/>



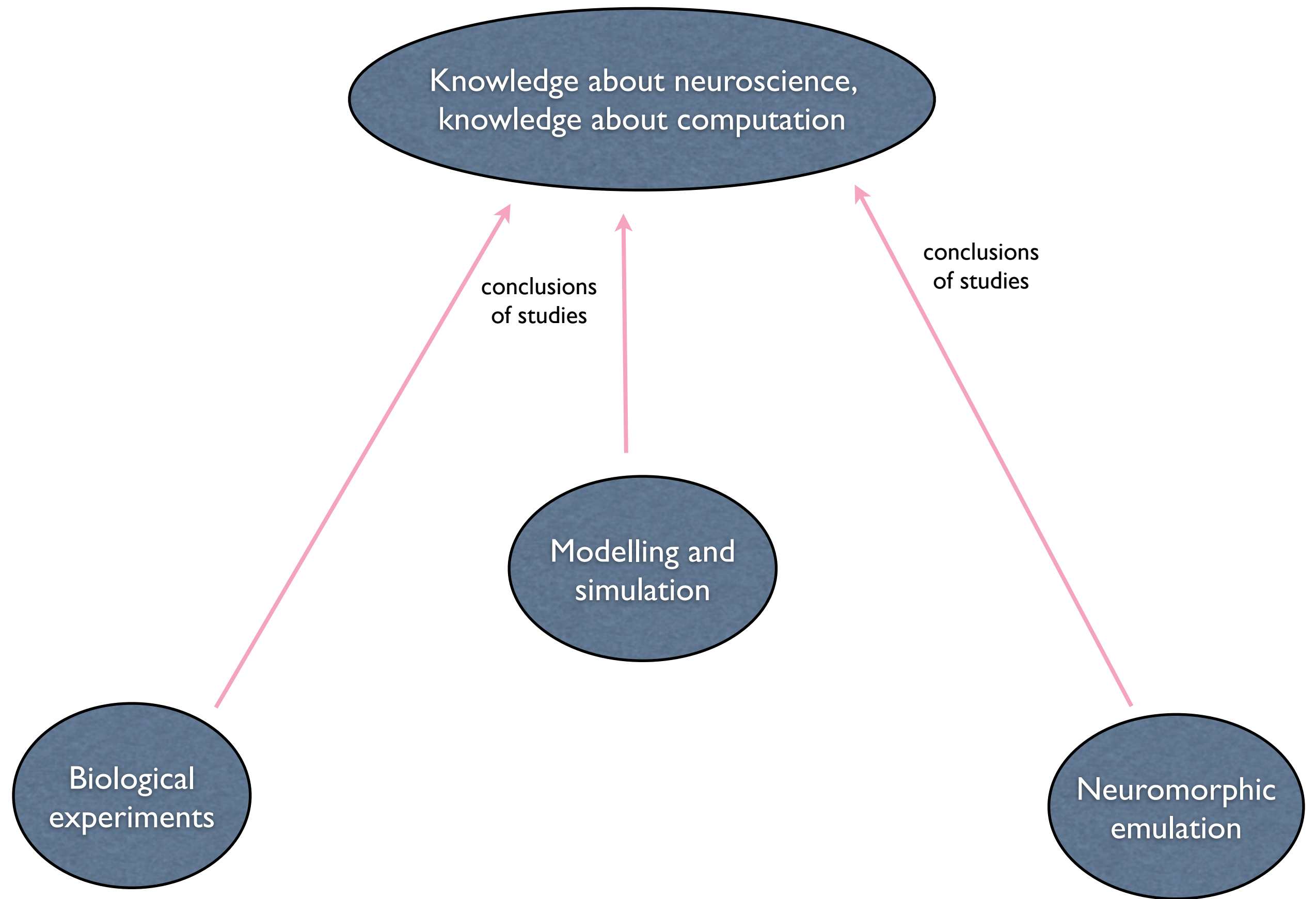
There are three fields represented within FACETS (and in neuromorphic computation in general). Most of the interaction between these domains takes place by exchange of knowledge, where I define knowledge as what we find in the Conclusions section of a paper. All three domains contribute to our collective knowledge about neuroscience and about computation. In turn, we use this knowledge in designing new experiments, new models, in designing new systems.

Knowledge about neuroscience,
knowledge about computation

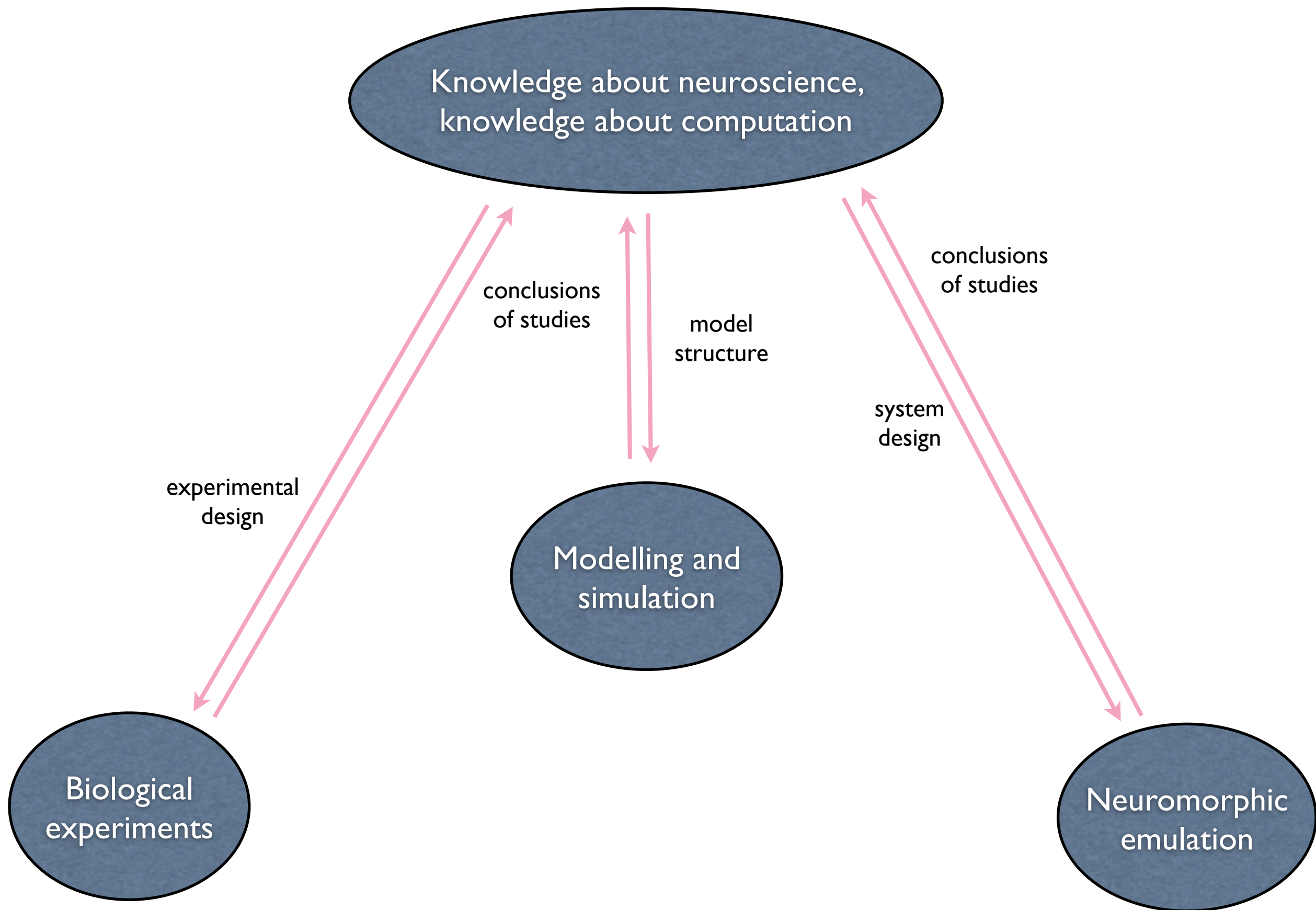
Modelling and
simulation

Biological
experiments

Neuromorphic
emulation

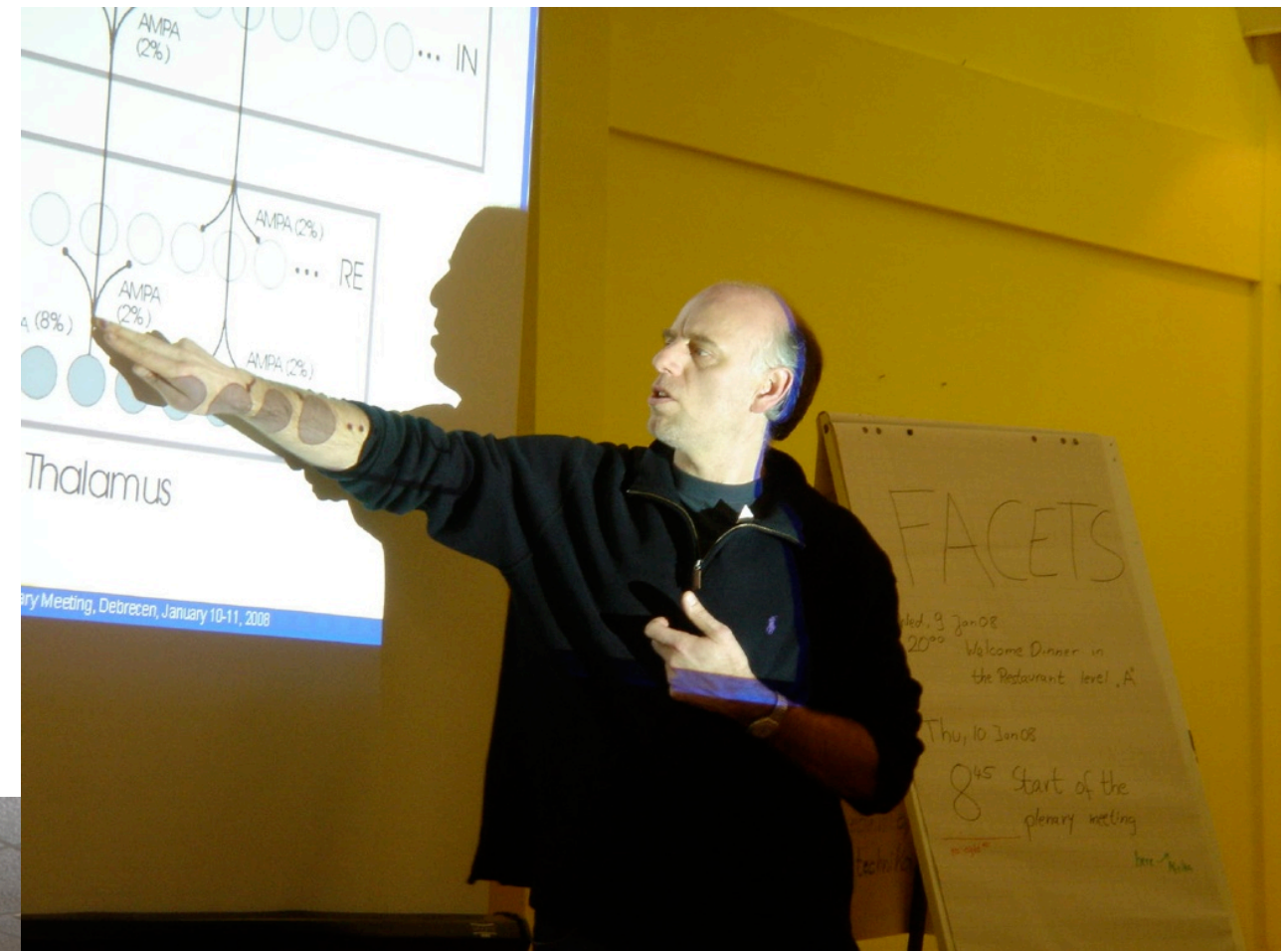
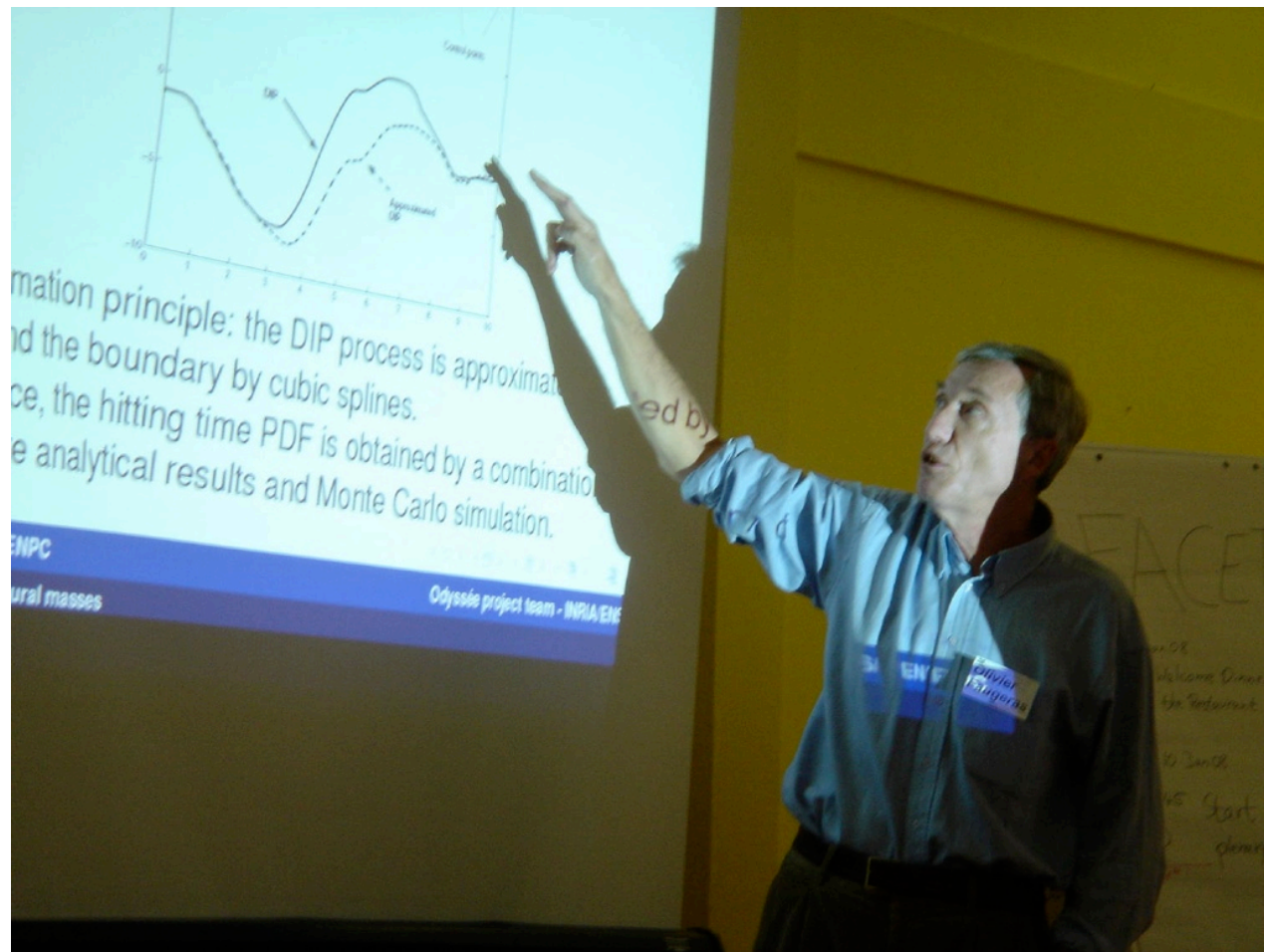


There are three fields represented within FACETS (and in neuromorphic computation in general). Most of the interaction between these domains takes place by exchange of knowledge, where I define knowledge as what we find in the Conclusions section of a paper. All three domains contribute to our collective knowledge about neuroscience and about computation. In turn, we use this knowledge in designing new experiments, new models, in designing new systems.



There are three fields represented within FACETS (and in neuromorphic computation in general). Most of the interaction between these domains takes place by exchange of knowledge, where I define knowledge as what we find in the Conclusions section of a paper. All three domains contribute to our collective knowledge about neuroscience and about computation. In turn, we use this knowledge in designing new experiments, new models, in designing new systems.

Knowledge flow



So how does this exchange of knowledge take place – of course it takes place from human-to-human, via meetings, papers, presentations. How well does the exchange work?

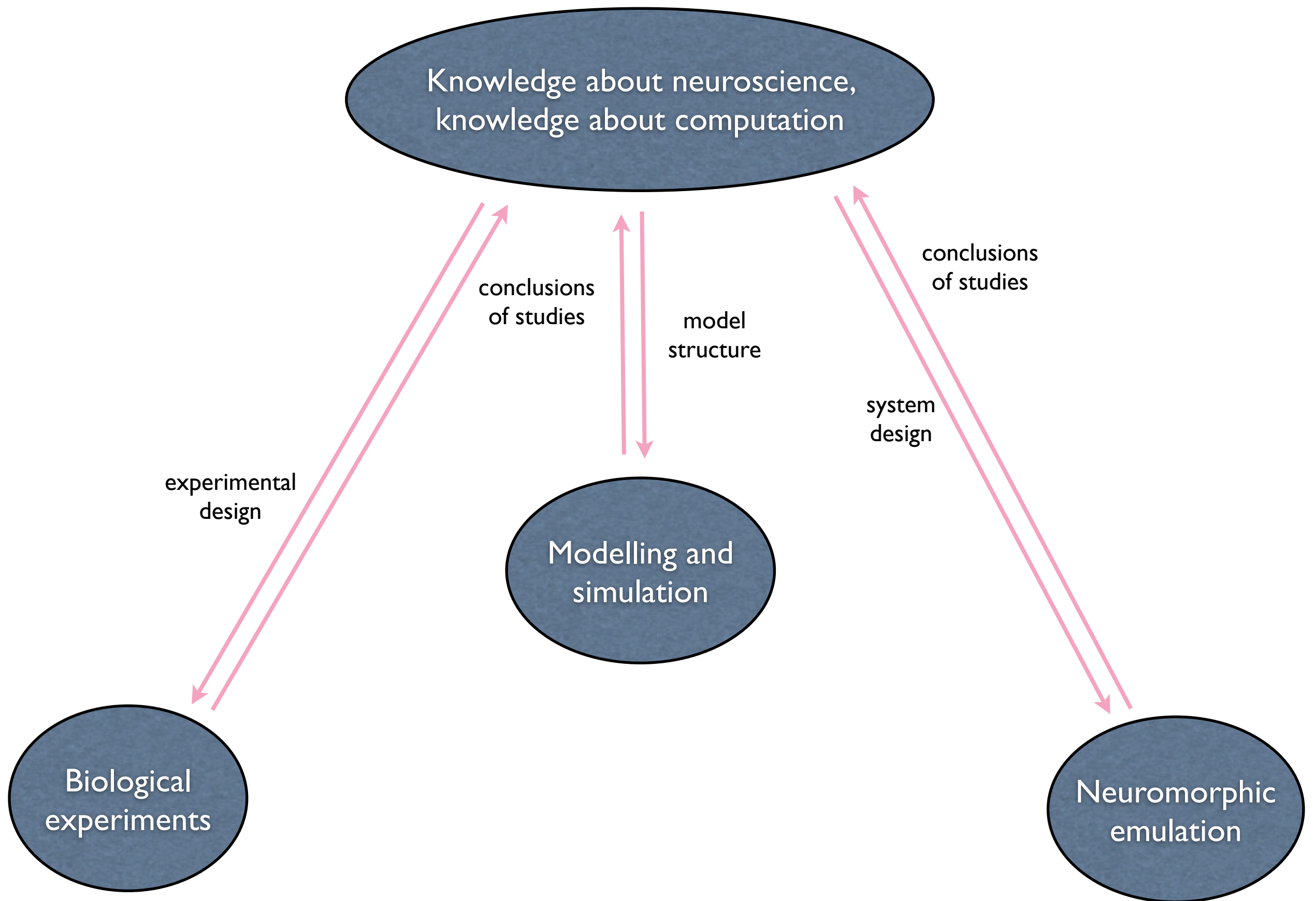
Knowledge flow: works fairly well*



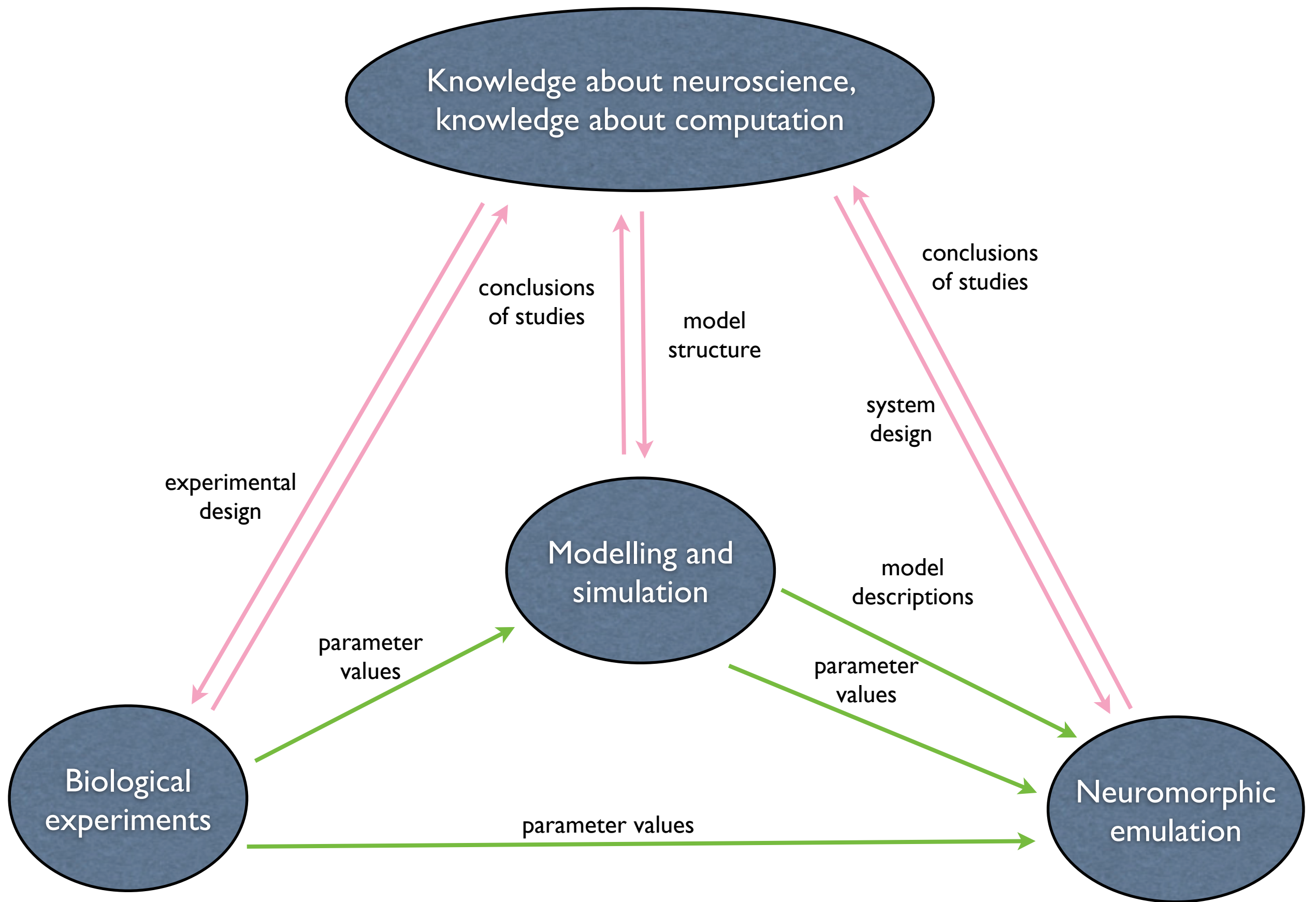
I 210 & 57 freeways by kla4067
<http://www.flickr.com/photos/84263554@N00/2078587948/>

* but see Science 2.0

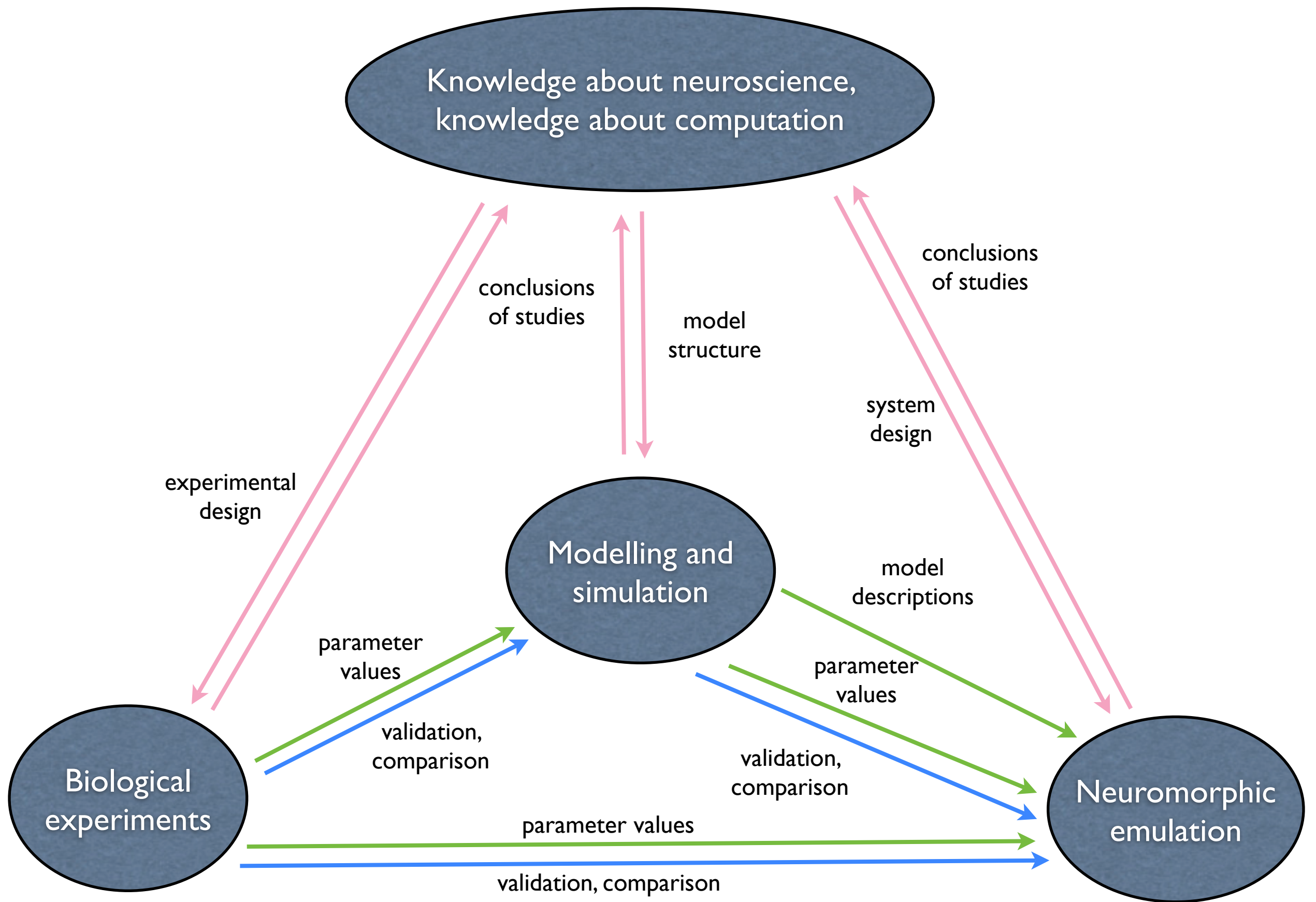
In general, it works fairly well – very well in the FACETS project – knowledge gets moved around fairly fast and effectively, even if some people think it could work a lot better (open-access publishing, semantic web, blog-based publishing, etc.)



But as well as the flow of knowledge, we also have flows of information (green lines) and of data (blue), where I define information as what goes into the Methods section of a paper: metadata might be a better word. So biological experiments can provide parameter values for models, and we can use data from experiments to test and attempt to validate our models and hardware.



But as well as the flow of knowledge, we also have flows of information (green lines) and of data (blue), where I define information as what goes into the Methods section of a paper: metadata might be a better word. So biological experiments can provide parameter values for models, and we can use data from experiments to test and attempt to validate our models and hardware.



But as well as the flow of knowledge, we also have flows of information (green lines) and of data (blue), where I define information as what goes into the Methods section of a paper: metadata might be a better word. So biological experiments can provide parameter values for models, and we can use data from experiments to test and attempt to validate our models and hardware.

Information and data flow

of the underlying V_m . We also find that the nonlinearities of the CRF are present at the level of V_m . Finally, we find that the variation in firing rates among cells can be accounted for by the different slopes of the linear relationships between V_m and the spike rate.

Materials and Methods

Surgical protocol. Experiments were conducted in accordance with the ethical guidelines of the National Institutes of Health and with the approval of the Institutional Animal Care and Use Committee of the University of Pennsylvania. Adult cats (2.5–3.5 kg) were anesthetized with an initial intraperitoneal injection of thiopental (25 mg/kg). Supplementary halothane (2–4% in a 70:30 mixture of N_2O and O_2) permitted the placement of two venous catheters. Subsequently, deep anesthesia was maintained during surgery with intravenous thiopental as needed and maintained for the duration of the experiment (14–16 hr) with a continuous infusion (3–10 mg/hr). Atropine sulfate (0.05 mg/kg, i.m.) was administered to prevent secretions and dexamethasone (4 mg, i.m.) to prevent cerebral edema. Lidocaine (2%) was generously applied to all skin incisions and pressure points. The animal was paralyzed with gallamine triethiodide (Flaxedil) by an initial injection of 60 mg and maintained with continuous intravenous infusion (20 mg/hr). The level of anesthesia was determined by continuously monitoring the EEG and the heart rate. Because the thiopental is infused continuously, we obtained very stable patterns of anesthesia throughout the experiment. The end-tidal CO_2 concentration was kept at $3.7 \pm 0.2\%$, and the rectal temperature was kept at $37\text{--}38^\circ C$ with a heating pad.

The surface of the visual cortex was exposed with a craniotomy centered at Horsley Clarke posterior 4.0, lateral 2.0 and bathed in mineral oil to prevent desiccation. The stability of the recordings was ensured by performing a bilateral pneumothorax, drainage of the cisterna magna, hip suspension, and by filling the cranial defect with a solution of 4% agar.

Visual stimulation. The corneas were protected with neutral contact lenses after dilating the pupils with 1% ophthalmic atropine and retracting the nictitating membranes with phenylephrine (Neosynephrine). Spectacle lenses were chosen by the tapetal reflection technique to optimize the focus of stimuli on the retina. The position of the monitor was adjusted with an x - y -stage so that the area centralae were well centered on the screen and their coordinates entered into the computer for tracking receptive field (RF) positions in retinal coordinates.

Stimuli were presented on an Image Systems (Minnetonka, MN) model M09LV monochrome monitor operating at 125 frames per second at a spatial resolution of 1024×786 pixels and a mean luminance of 47 cd/m^2 . The screen subtends 36 by 27° (28.7 pixels per degree), and lookup tables were linearized for a contrast range of $\pm 100\%$. Stimuli were synthesized using custom software by means of the framstore portion of a Cambridge Research Systems (Cambridge, UK) VSG card mounted in a conventional personal computer. Programs provide for stimulus control, online displays of acquired signals (V_m and spikes), and a graphical user interface for controlling all stimulus parameters. In addition to this online control, all data were stored on a Nicolet Vision, and it was from these records that offline analyses were performed. V_m and stimulus marks were sampled at 10 kHz with 16 bit analog-to-digital converters.

Computer-assisted hand plotting routines were used with every cell to estimate quickly and accurately the optimal orientation, direction, and spatial and temporal frequencies and to determine the receptive field position and dimensions. Contrast response functions were generated by presenting sinusoidal gratings of optimal orientation, direction, and spatial frequency, drifting within a patch limited to the receptive field. Mean luminance and all parameters of the stimuli were held constant except for

presentations at each contrast, and 5–15 passes were used for each contrast. Contrasts used were always 0, 2, 4, 8, 16, 32, and 64%.

Simple cells were distinguished from complex cells by the lack of spatial modulation of their spike trains. If the fundamental spatial frequency of the grating equaled or exceeded the DC, the cell was classified as simple (S); otherwise it was classified as complex.

Intracellular recording procedures. Intracellular recordings were obtained from the visual cortex as close as possible to the area centralis (P4, L2). Intracellular recordings were made using glass micropipettes filled with 2 M potassium acetate (KOH and acetate added). The depth of the cells was estimated by recording, which was calibrated by comparing the depths of cells filled with Neurobiotin ($n = 12$) and error. After beveling, pipettes had final resistances of $100\text{--}200 \text{ M}\Omega$.

Statistical analysis. Contrast response functions were fitted using MatLab (MathWorks, Natick, MA). Spike firing rates were determined from the Nicolet records, and PSTHs were generated. Spike counts per bin ($n = 100$) evenly spaced over the range of contrast. F1 and DC response components were extracted from the stimulus histograms (PSTHs) at each contrast on the basis of the F1 and DC components. Spikes were also removed from the records of V_m (to avoid contamination), and cyclegrams were generated of V_m for each contrast. F1 and DC components were extracted from the V_m cyclegrams. F1 terms and seven DC terms were obtained for both V_m and spike counts. Each set of 4×7 observations was fit to the data using the Levenberg–Marquardt method to minimize the sum of squares between the observations and the candidate function. The method combines the steepest-descent method and a Taylor series expansion to obtain a fast, reliable technique for nonlinear optimization. The lead of Albrecht and Hamilton (1982), the four parameters are:

Linear $R(C) = a + b \cdot C$,
 Log $R(C) = a + b \cdot \log_{10}(C)$,
 Power $R(C) = a + b \cdot C^c$,
 Hyperbolic ratio $R(C) = R_{\max} \cdot C^n / (C_{50}^n + C^n)$,
 where $R(C)$ denotes response as a function of contrast C , and activity (or resting V_m) was subtracted from the data. The parameters of the hyperbolic ratio function were fitted to the data.

Results. In most instances, the groups being compared are compared using nonparametric statistics are used unless otherwise noted.

Results

Our goal was to characterize quantitatively the trophologically defined cell classes in primary visual cortex as a function of the contrast of visual stimuli. Using intracellular recording *in vivo*, we measured the responses to sinusoidal gratings of optimal orientation and spatiotemporal frequency presented at logarithmically spaced contrasts. We characterized electrophysiologically with intracellular recordings and contrast response functions (CRFs) were obtained for simple and complex cells (in Hertz). The CRFs were characterized by least-squares fits to four mathematical functions: linear, logarithmic, power, and hyperbolic ratio (see Methods). The parameters of these fits were used to compare the CRFs obtained simultaneously for simple and complex cells and to summarize and compare the responses of the different cell classes. We emphasize the differences between simple and complex cells because they constitute the great majority of inhibitory cells in the neocortex, but we also show



Now, at the moment, data flows between scientists mostly via zip files, e-mail attachments, DVDs. Information – metadata – mostly flows via the same route as knowledge, via PDFs.

Information and data flow: doesn't work quite so well



Horse & Cart at the Muslim Cemetery, Tetovo by themanwithsalhair
<http://www.flickr.com/photos/themanwithsalhair/3038240771/>

This is not so good. We have format problems, data going missing, multiple slightly different copies... (see <http://www.phdcomics.com/comics.php?f=1323>)

Information and data flow: doesn't work quite so well

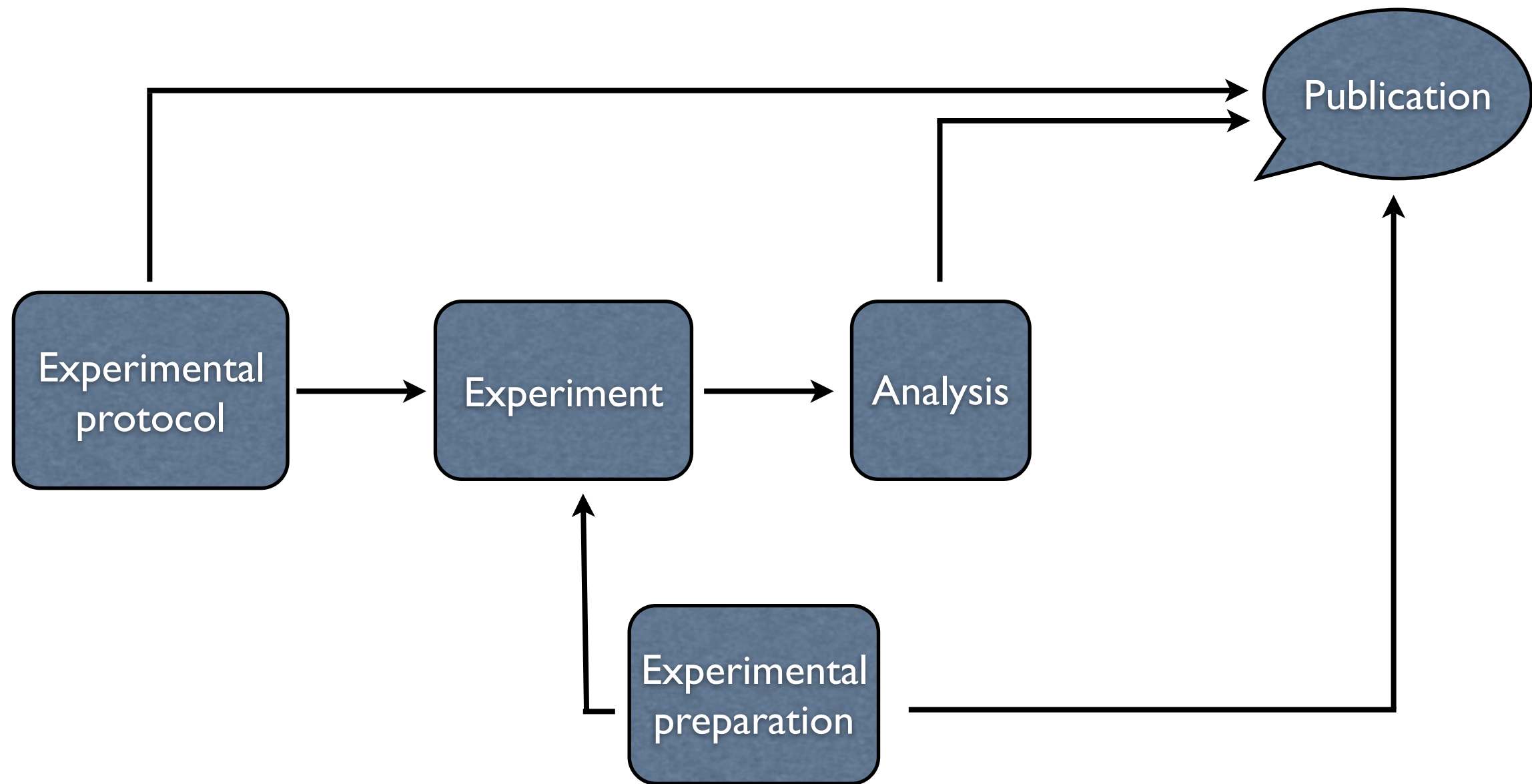


Frozen waterfall by ingermaaike2
<http://www.flickr.com/photos/ingermaaike2/4318204427/>

and information doesn't flow at all; Or only flows via the knowledge pathways (papers, PDFs) and with very lossy transmission.

To recap: neuromorphic computation requires effective and rapid communication of knowledge, information, and data between biologists, physicists, engineers, ... but while knowledge flow works well, there are problems with exchanging information and data. So one of the goals of FACETS was to improve the flow of data and of information between the different groups and disciplines within the project.

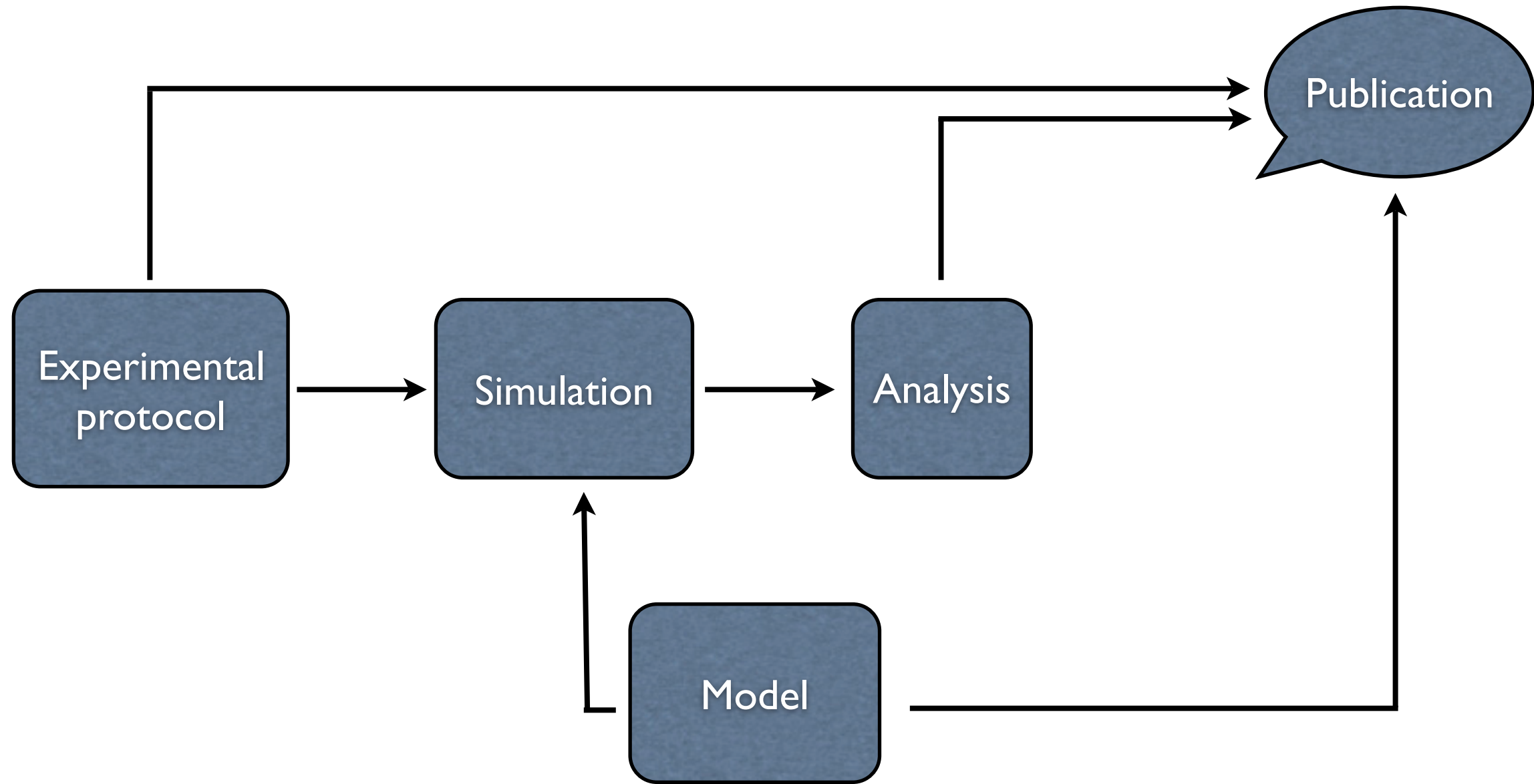
Experimental workflow



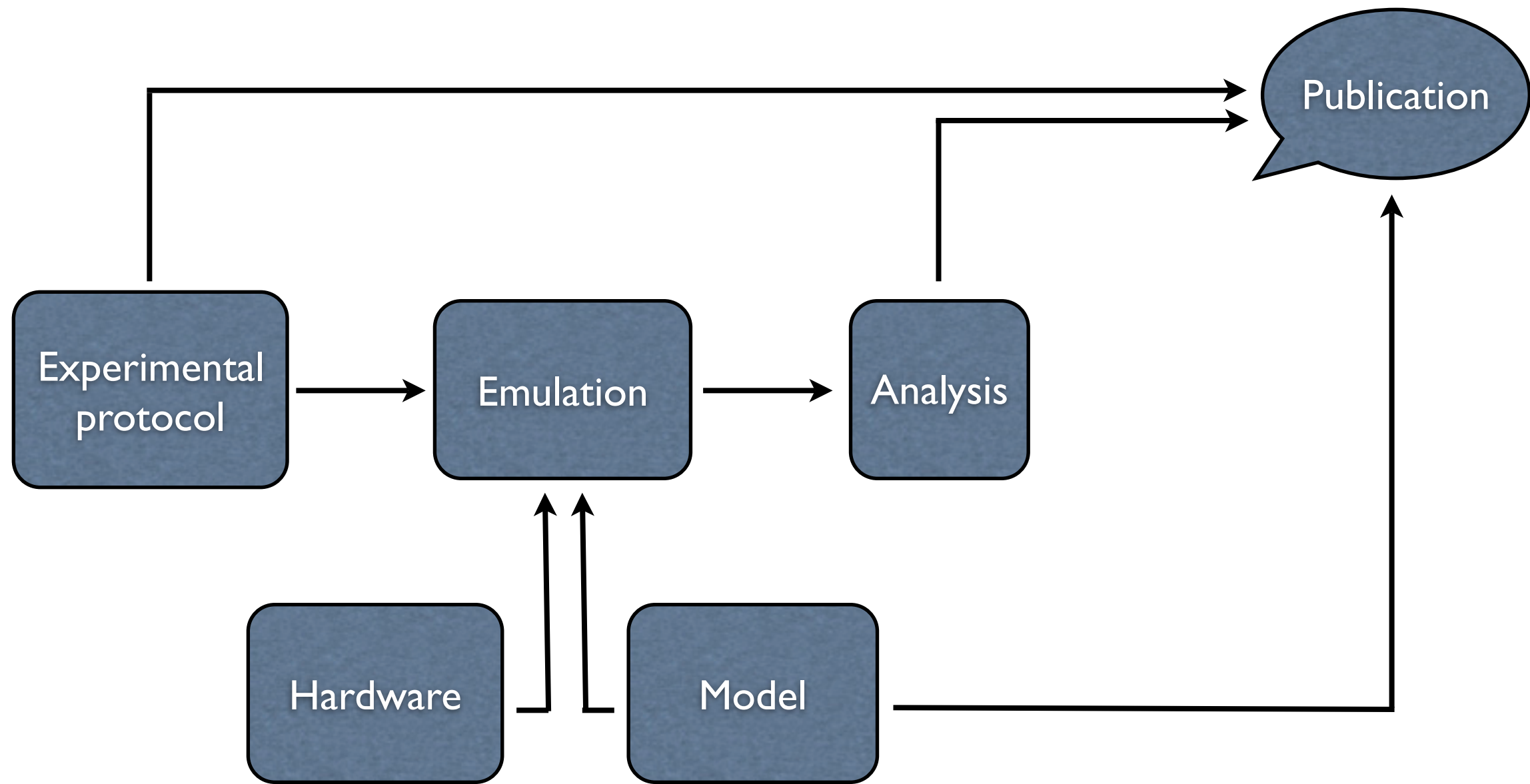
Now I'm going to present some of the tools we developed for improving data/information flow in FACETS.
To be more precise about the types of data and information we're interested in, I want to consider some typical workflows in FACETS.

The workflows for biological experiments, ...

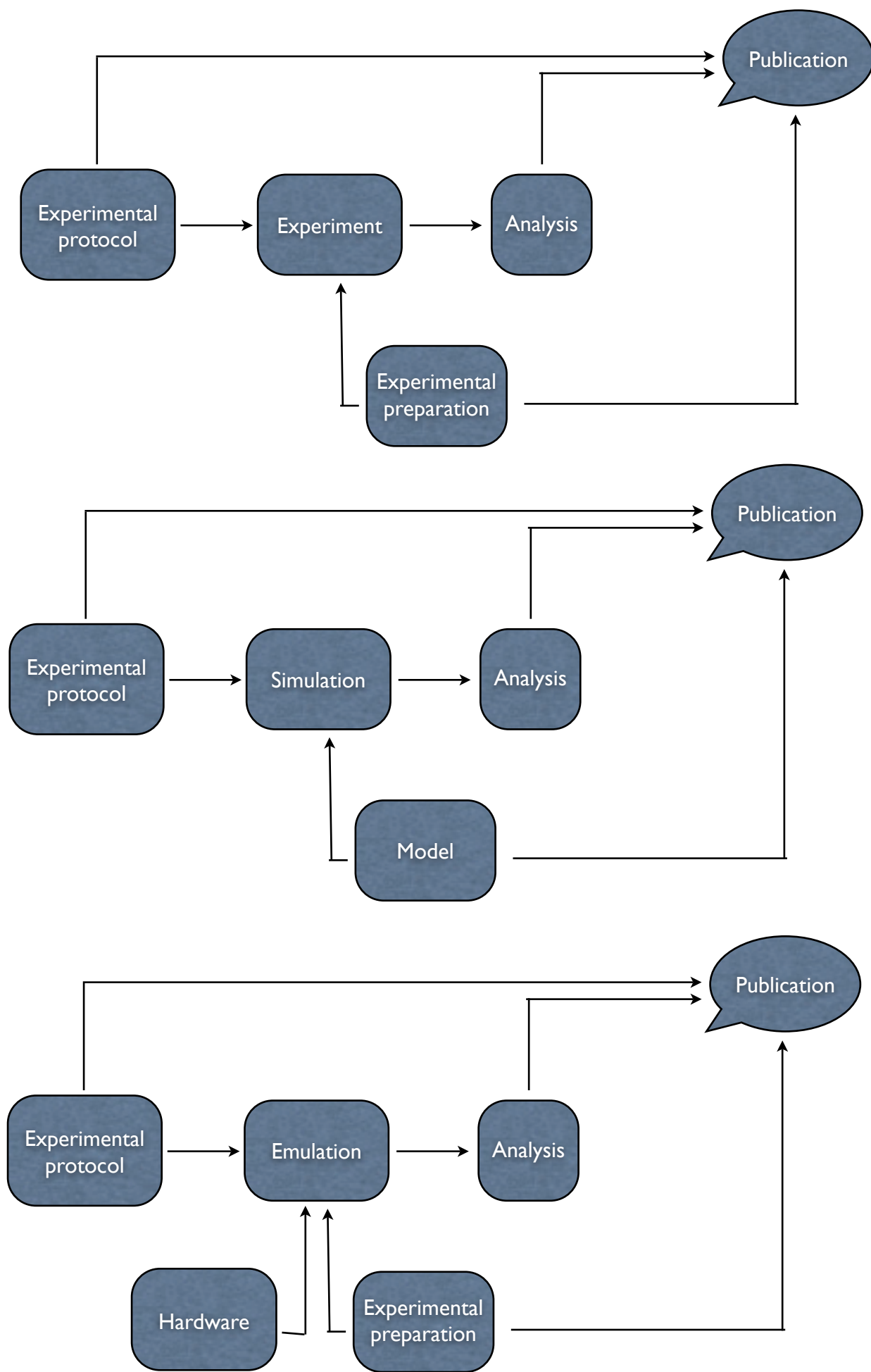
Software simulation workflow



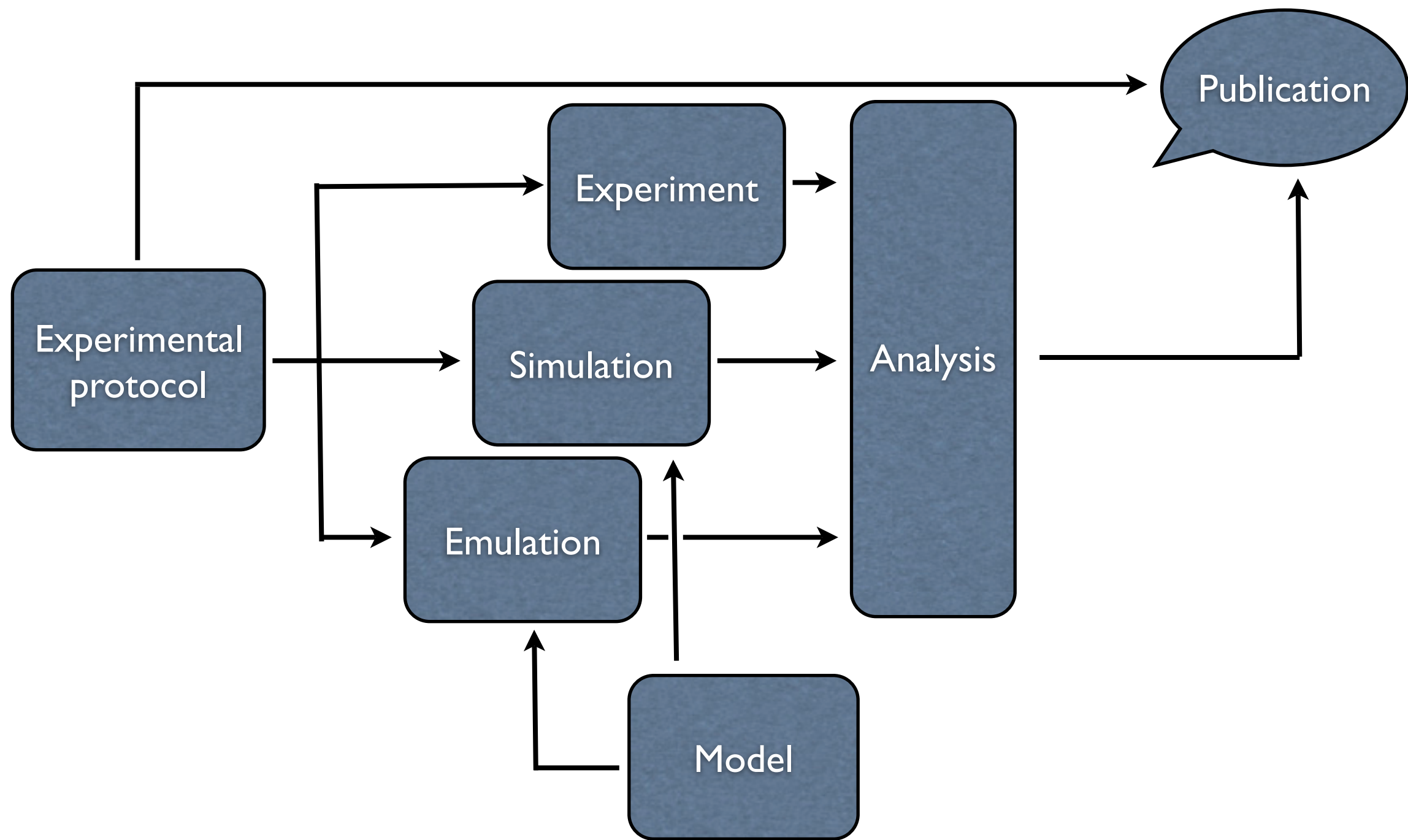
Hardware emulation workflow



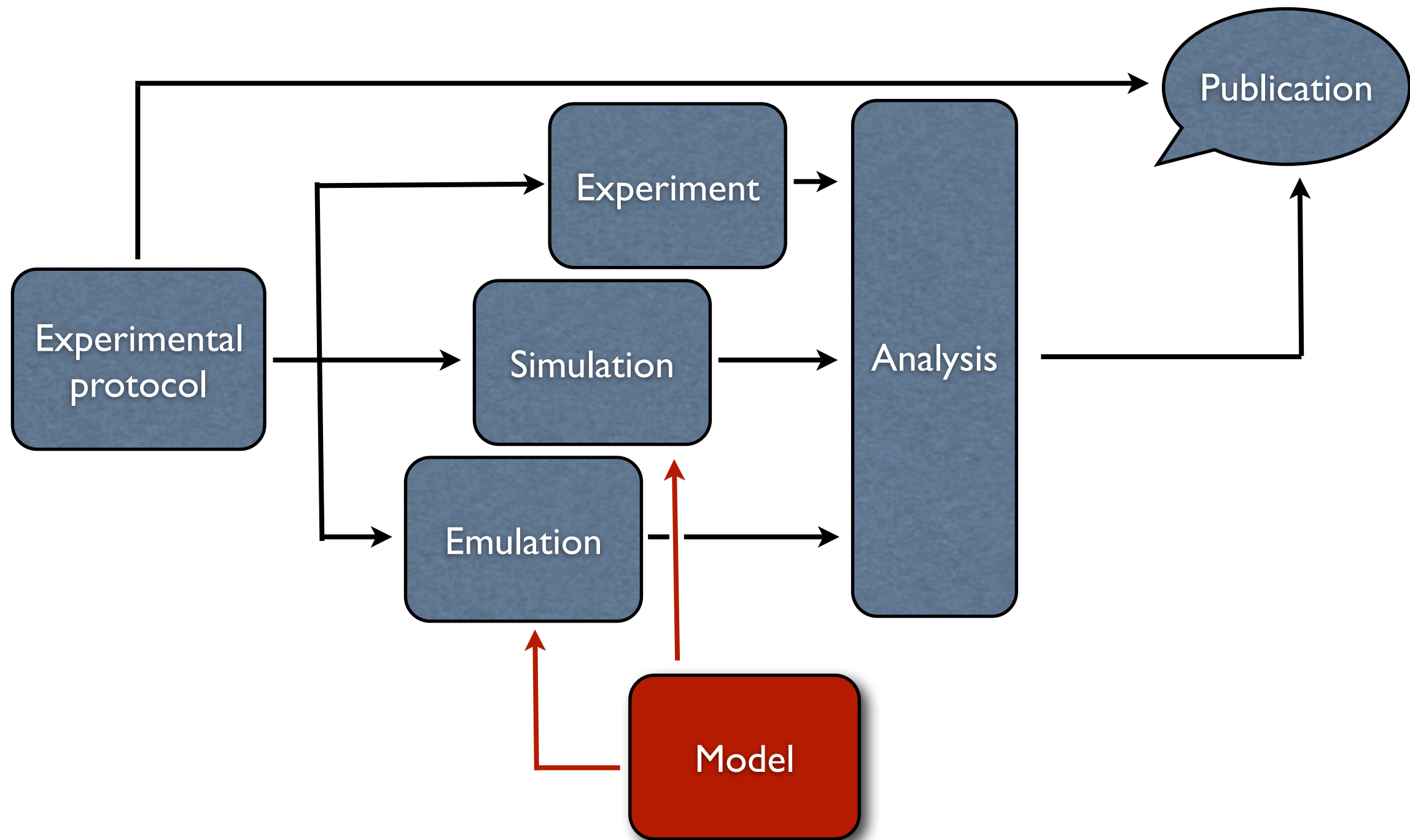
... and for running experiments on the hardware (as Daniel Brüderle showed yesterday) are all very similar.



So there are evident redundancies here, and if we wish to compare experiments, software simulations and hardware emulations, there are several barriers.



A common interface for model descriptions



In neuroscience, models often live in a walled garden

- not reproducible from published descriptions
- only run on a single simulator
- hence not testable or reusable

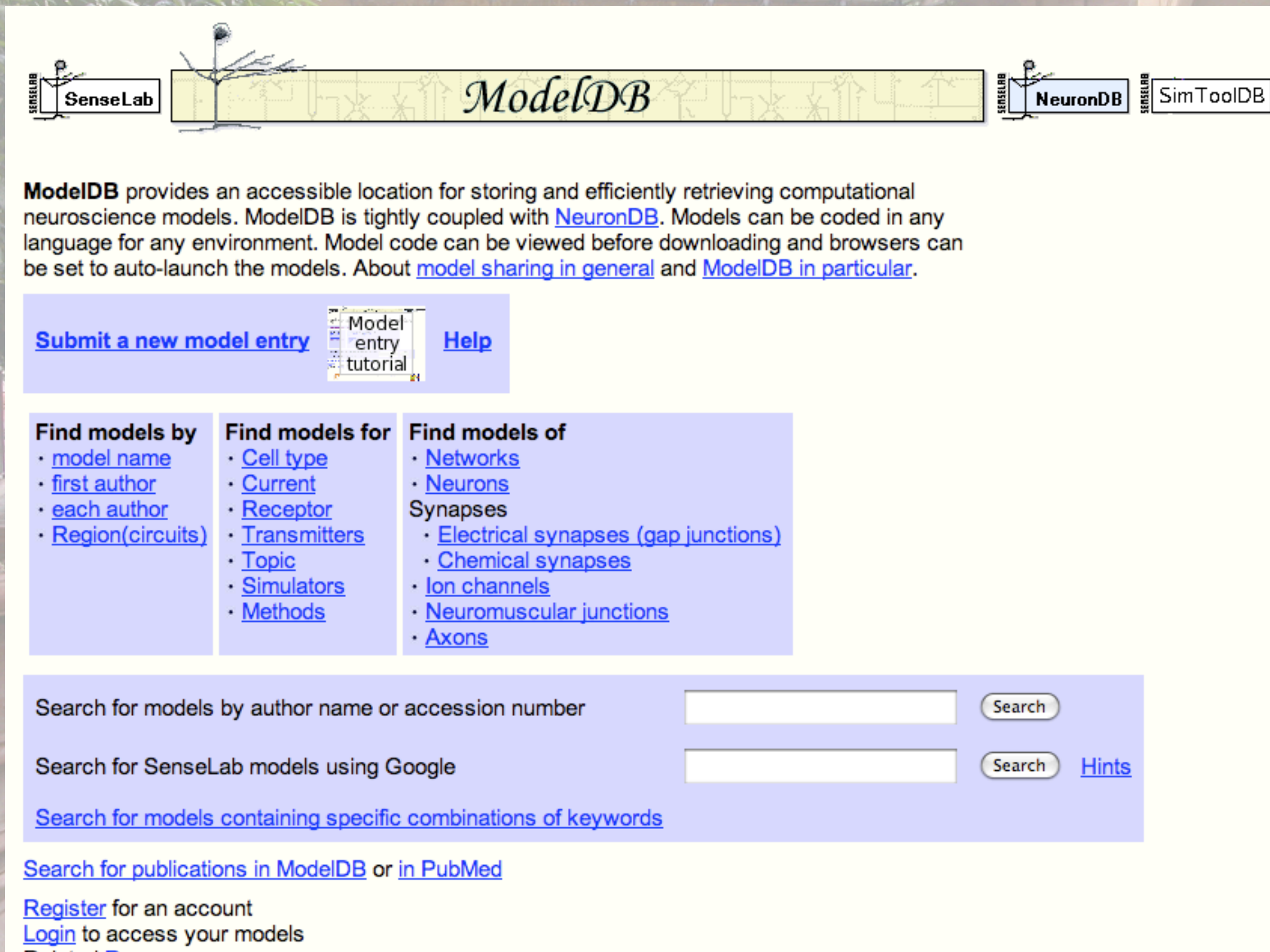
Solution 1: improve published descriptions

- improve the papers:
 - E. Nordlie and H. E. Plesser. Visualizing neuronal network connectivity with connectivity pattern tables. *Front. Neuroinform.*, 3:39, 2010. DOI 10.3389/neuro.11.039.2009.
 - E. Nordlie, M.-O. Gewaltig, and H. E. Plesser. Towards reproducible descriptions of neuronal network models. *PLoS Comput Biol*, 5(8):e1000456, Aug 2009. DOI 10.1371/journal.pcbi.1000456.
- publish to a database:
 - machine-readable, declarative descriptions
 - widely used in systems biology (SBML, CellML, SED-ML, BioModels database)
 - preliminary attempts in neuroscience: NeuroML, NineML.

There are 2 ways to improve this situation, and we need both.

One way is to improve the published descriptions.


Solution 2: get the code



The screenshot shows the ModelDB website header with logos for SenseLab, ModelDB, NeuronDB, and SimToolDB. Below the header is a paragraph describing ModelDB's purpose and linking to NeuronDB. A navigation bar contains links for 'Submit a new model entry', a 'Model entry tutorial' icon, and 'Help'. Three columns of search filters are provided: 'Find models by' (model name, first author, each author, Region), 'Find models for' (Cell type, Current, Receptor, Transmitters, Topic, Simulators, Methods), and 'Find models of' (Networks, Neurons, Synapses, Electrical synapses, Chemical synapses, Ion channels, Neuromuscular junctions, Axons). A search section includes three input fields with 'Search' buttons and a 'Hints' link. At the bottom, there are links for 'Search for publications in ModelDB or in PubMed', 'Register for an account', and 'Login to access your models'.

SenseLab **ModelDB** **NeuronDB** **SimToolDB**

ModelDB provides an accessible location for storing and efficiently retrieving computational neuroscience models. ModelDB is tightly coupled with [NeuronDB](#). Models can be coded in any language for any environment. Model code can be viewed before downloading and browsers can be set to auto-launch the models. About [model sharing in general](#) and [ModelDB in particular](#).

[Submit a new model entry](#)  [Help](#)

Find models by

- [model name](#)
- [first author](#)
- [each author](#)
- [Region\(circuits\)](#)

Find models for

- [Cell type](#)
- [Current](#)
- [Receptor](#)
- [Transmitters](#)
- [Topic](#)
- [Simulators](#)
- [Methods](#)

Find models of

- [Networks](#)
- [Neurons](#)
- Synapses
 - [Electrical synapses \(gap junctions\)](#)
 - [Chemical synapses](#)
- [Ion channels](#)
- [Neuromuscular junctions](#)
- [Axons](#)

Search for models by author name or accession number

Search for SenseLab models using Google [Hints](#)

[Search for models containing specific combinations of keywords](#)

[Search for publications in ModelDB](#) or [in PubMed](#)

[Register](#) for an account
[Login](#) to access your models

Solution 2: get the code...and then translate it



Find Models by Simulation Environment

Click on a link to show a list of models implemented in that simulation environment or programming language.

Simulation Environment	Homepage	Number of models
BioPAX (web link to model)		1
Brian		4
C or C++ program		34
C or C++ program (web link to model)		19
CONTENT		1
CSIM		1
CSIM (web link to model)		3
CaC Calcium Calculator		1
CaC Calcium Calculator (web link to model)		7
Catacomb (web link to model)		1
CellExcite (web link to model)		1
CellML		0
CellML (web link to model)		1
Chemesis		2
Dynamics Solver		1
Emergent/PDP++		3
FORTRAN		4
FORTRAN (web link to a model)		1
GNUstep NeXTStep/OpenStep		1
Genesis		13
Genesis (web link to model)		7

... although even then, if you want to solve a model on a different simulator to the original one, or combine two models developed for different simulators, you're in for a tedious and difficult translation task.

Simulator diversity: problem and opportunity

Cons

- Considerable difficulty in translating models from one simulator to another...
- ...or even in understanding someone else's code.
- This:
 - impedes communication between investigators,
 - makes it harder to reproduce other people's work,
 - makes it harder to build on other people's work.

Pros

- Each simulator has a different balance between efficiency, flexibility, scalability and user-friendliness → can choose the most appropriate for a given problem.
- Any given simulator is likely to have bugs and hidden assumptions, which will be revealed by cross-checking results between different simulators → greater confidence in correctness of results.

Having your cake and eating it

Simulator-independent environments for developing neuroscience models:

- keep the advantages of having multiple simulators or hardware devices
- but remove the translation barrier.

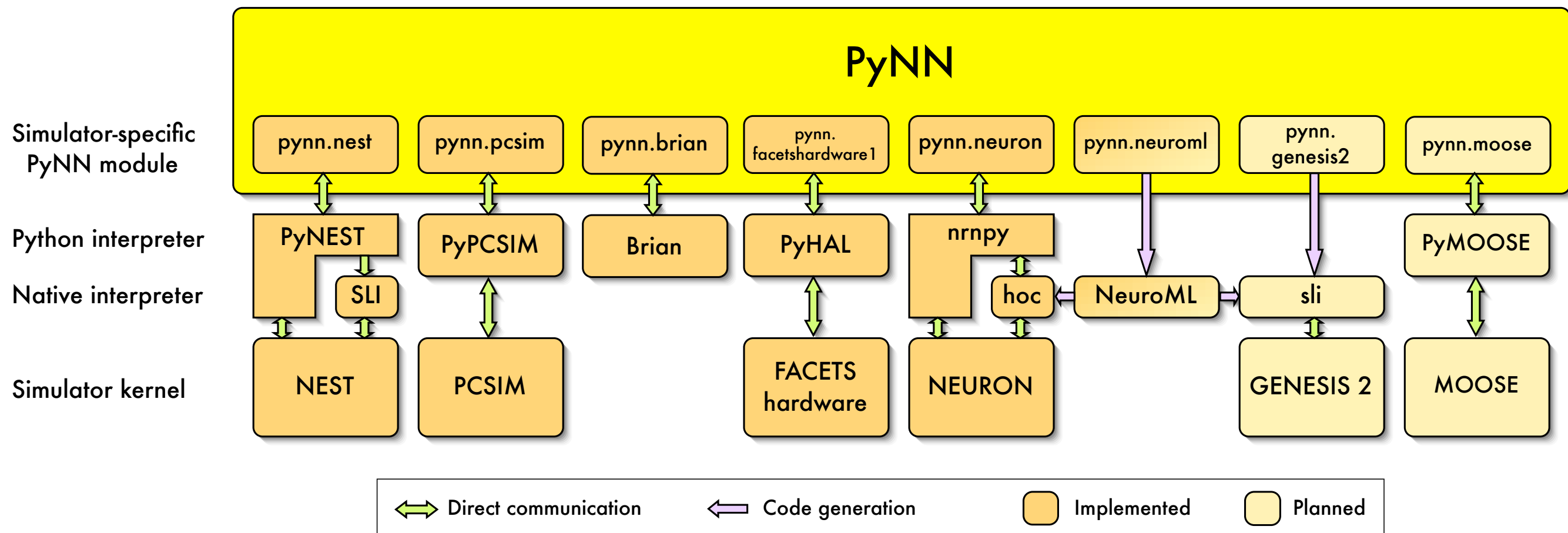
Three (complementary) approaches:

- GUI (e.g. neuroConstruct)
- XML-based language (e.g. NeuroML)
- interpreted language (e.g. Python)



Cawan Cake by Nono Fara <http://www.flickr.com/photos/n-o-n-o/3280580620/>

PyNN: write the code for a simulation once, run it on any supported simulator or hardware device *without modification*.



<http://neuralensemble.org/PyNN>

```

sim.setup(timestep=0.1)
cell_parameters = {"tau_m": 12.0, "cm": 0.8, "v_thresh": -50.0,
                  "v_reset": -65.0}
pE = sim.Population((100,100), sim.IF_cond_exp, cell_parameters,
                  label="excitatory neurons")
pI = sim.Population((50,50), sim.IF_cond_exp, cell_parameters,
                  label="inhibitory neurons")
input = sim.Population(100, sim.SpikeSourcePoisson)
rate_distr = random.RandomDistribution("normal", (10.0, 2.0))
input.rset("rate", rate_distr)
background = sim.NoisyCurrentSource(mean=0.1, stdev=0.01)
pE.inject(background)
pI.inject(background)
DDPC = sim.DistanceDependentProbabilityConnector
weight_distr = random.RandomDistribution("uniform", (0.0, 0.1))
connector = DDPC("exp(-d**2/400.0)", weights=weight_distr,
                delays="0.5+0.01d")
TMM = sim.TsodyksMarkramMechanism
depressing = sim.DynamicSynapse(fast=TMM(U=0.5, tau_rec=800.0))
e2e = sim.Projection(pE, pE, connector, target="excitatory",
                    synapse_dynamics=plasticity)
e2i = sim.Projection(pE, pI, connector, target="excitatory")
i2e = sim.Projection(pI, pE, connector, target="inhibitory")

```



```

import pyNN.neuron as sim
sim.setup(timestep=0.1)
cell_parameters = {"tau_m": 12.0, "cm": 0.8, "v_thresh": -50.0,
                  "v_reset": -65.0}
pE = sim.Population((100,100), sim.IF_cond_exp, cell_parameters,
                  label="excitatory neurons")
pI = sim.Population((50,50), sim.IF_cond_exp, cell_parameters,
                  label="inhibitory neurons")
input = sim.Population(100, sim.SpikeSourcePoisson)
rate_distr = random.RandomDistribution("normal", (10.0, 2.0))
input.rset("rate", rate_distr)
background = sim.NoisyCurrentSource(mean=0.1, stdev=0.01)
pE.inject(background)
pI.inject(background)
DDPC = sim.DistanceDependentProbabilityConnector
weight_distr = random.RandomDistribution("uniform", (0.0, 0.1))
connector = DDPC("exp(-d**2/400.0)", weights=weight_distr,
                delays="0.5+0.01d")
TMM = sim.TsodyksMarkramMechanism
depressing = sim.DynamicSynapse(fast=TMM(U=0.5, tau_rec=800.0))
e2e = sim.Projection(pE, pE, connector, target="excitatory",
                    synapse_dynamics=plasticity)
e2i = sim.Projection(pE, pI, connector, target="excitatory")
i2e = sim.Projection(pI, pE, connector, target="inhibitory")

```

```

import pyNN.nest as sim
sim.setup(timestep=0.1)
cell_parameters = {"tau_m": 12.0, "cm": 0.8, "v_thresh": -50.0,
                  "v_reset": -65.0}
pE = sim.Population((100,100), sim.IF_cond_exp, cell_parameters,
                  label="excitatory neurons")
pI = sim.Population((50,50), sim.IF_cond_exp, cell_parameters,
                  label="inhibitory neurons")
input = sim.Population(100, sim.SpikeSourcePoisson)
rate_distr = random.RandomDistribution("normal", (10.0, 2.0))
input.rset("rate", rate_distr)
background = sim.NoisyCurrentSource(mean=0.1, stdev=0.01)
pE.inject(background)
pI.inject(background)
DDPC = sim.DistanceDependentProbabilityConnector
weight_distr = random.RandomDistribution("uniform", (0.0, 0.1))
connector = DDPC("exp(-d**2/400.0)", weights=weight_distr,
               delays="0.5+0.01d")
TMM = sim.TsodyksMarkramMechanism
depressing = sim.DynamicSynapse(fast=TMM(U=0.5, tau_rec=800.0))
e2e = sim.Projection(pE, pE, connector, target="excitatory",
                  synapse_dynamics=plasticity)
e2i = sim.Projection(pE, pI, connector, target="excitatory")
i2e = sim.Projection(pI, pE, connector, target="inhibitory")

```

```

import pyNN.hardware.facets.stagel as sim
sim.setup(timestep=0.1)
cell_parameters = {"tau_m": 12.0, "cm": 0.8, "v_thresh": -50.0,
                  "v_reset": -65.0}
pE = sim.Population((100,100), sim.IF_cond_exp, cell_parameters,
                  label="excitatory neurons")
pI = sim.Population((50,50), sim.IF_cond_exp, cell_parameters,
                  label="inhibitory neurons")
input = sim.Population(100, sim.SpikeSourcePoisson)
rate_distr = random.RandomDistribution("normal", (10.0, 2.0))
input.rset("rate", rate_distr)
background = sim.NoisyCurrentSource(mean=0.1, stdev=0.01)
pE.inject(background)
pI.inject(background)
DDPC = sim.DistanceDependentProbabilityConnector
weight_distr = random.RandomDistribution("uniform", (0.0, 0.1))
connector = DDPC("exp(-d**2/400.0)", weights=weight_distr,
                delays="0.5+0.01d")
TMM = sim.TsodyksMarkramMechanism
depressing = sim.DynamicSynapse(fast=TMM(U=0.5,tau_rec=800.0))
e2e = sim.Projection(pE, pE, connector, target="excitatory",
                    synapse_dynamics=plasticity)
e2i = sim.Projection(pE, pI, connector, target="excitatory")
i2e = sim.Projection(pI, pE, connector, target="inhibitory")

```

This is how you run it on the FACETS neuromorphic hardware.

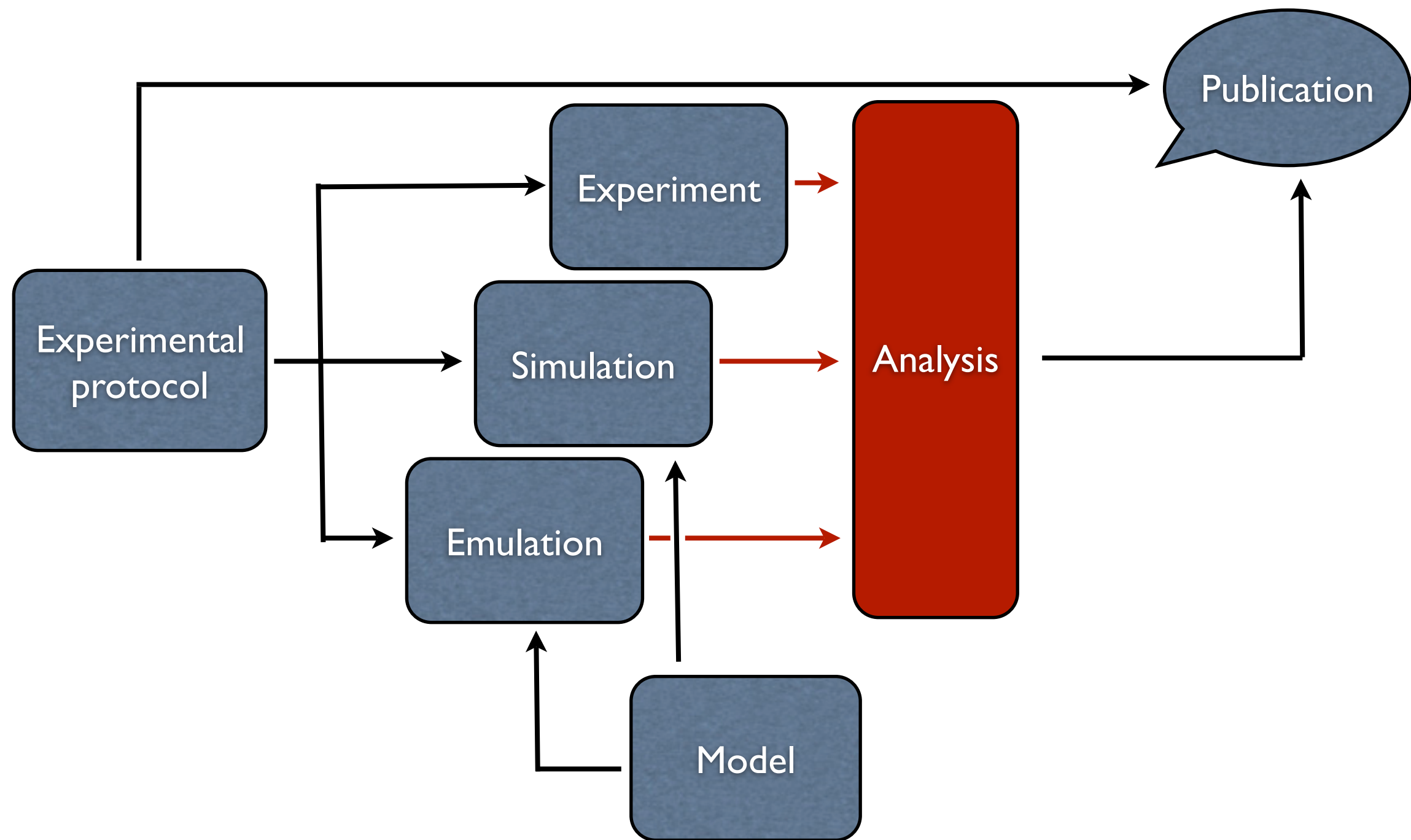
So once you've defined your model, you can choose to run it on the simulator that fits it best, and you can check that different simulators give the same result, and, as Daniel Brüderle demonstrated yesterday, you can also transfer your model trivially to neuromorphic hardware.

<http://neuralensemble.org/PyNN>

Davison A.P., Brüderle D., Eppler J.M., Kremkow, J., Müller E., Pecevski D.A., Perrinet L. and Yger P. (2009) PyNN: a common interface for neuronal network simulators. *Frontiers in Neuroinformatics* 2:11: doi:10.3389/neuro.11.011.2008

Brüderle D., Müller E., Davison A., Müller E., Schemmel J. and Meier K. (2009) Establishing a Novel Modeling Tool: A Python-based Interface for a Neuromorphic Hardware System. *Frontiers in Neuroinformatics* 3:17: doi:10.3389/neuro.11.017.2009

A shared toolbox for analysis and visualisation



Parallel reimplementation of analysis routines by generations of PhD students...



FIND

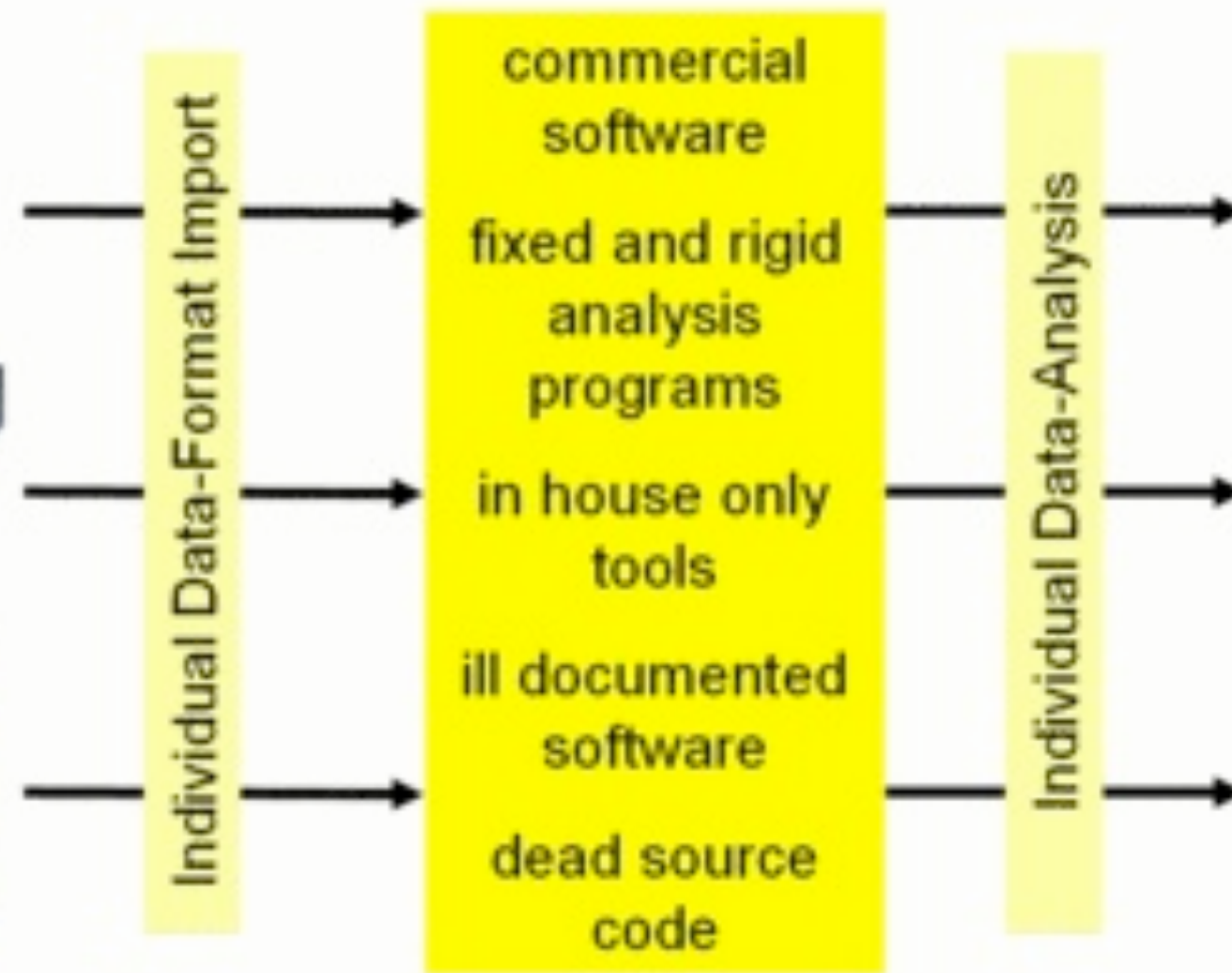
Finding Information in Neural Data



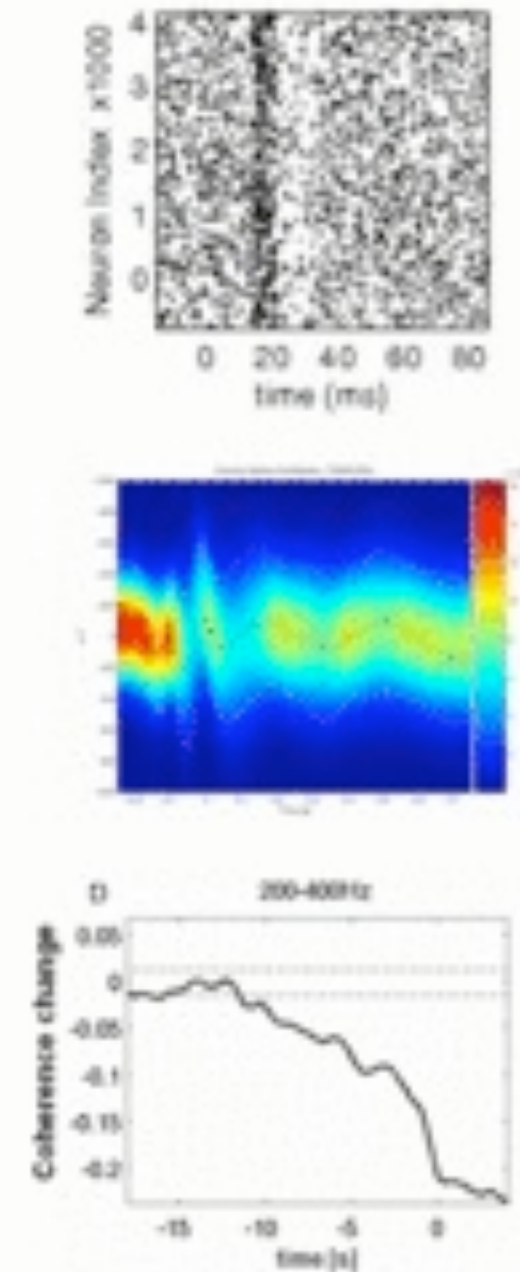
Data Acquisition and Generation



Analysis Tools



Results



Ralph Meier, BCCN Freiburg

FIND

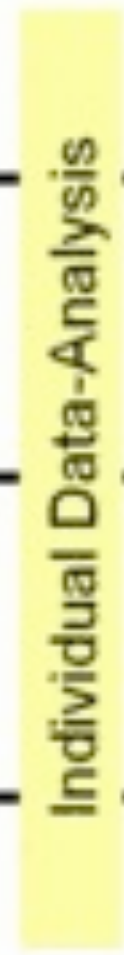
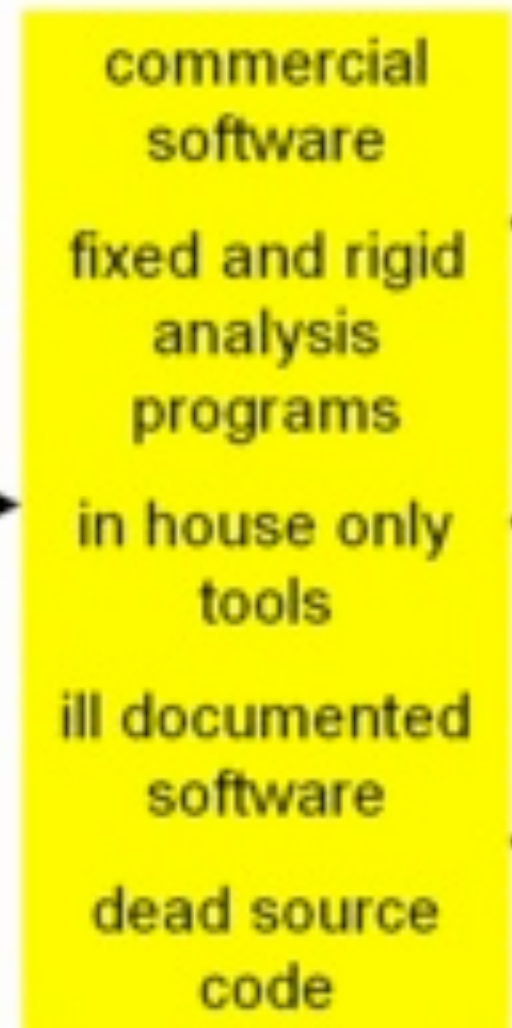
Finding Information in Neural Data using NeuroShare



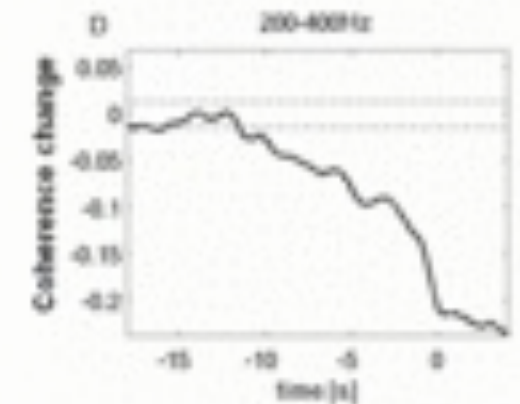
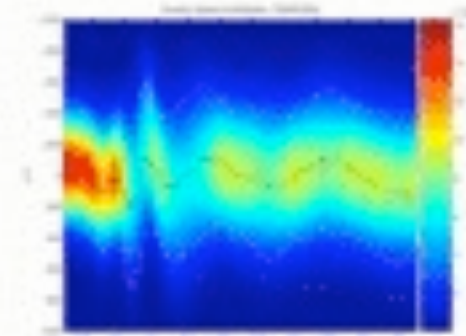
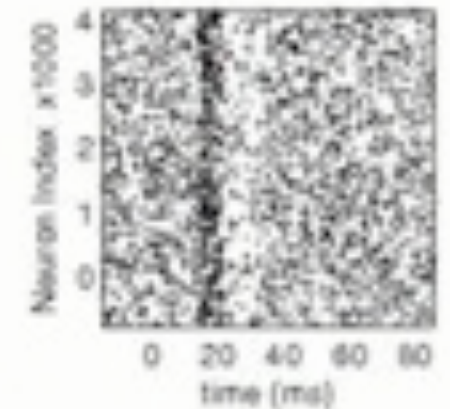
Data Acquisition and Generation



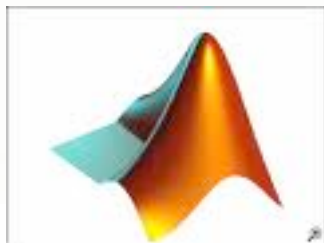
Analysis Tools



Results



Ralph Meier, BCCN Freiburg



FIND

Finding Information in Neural Data – Toolbox using NeuroShare

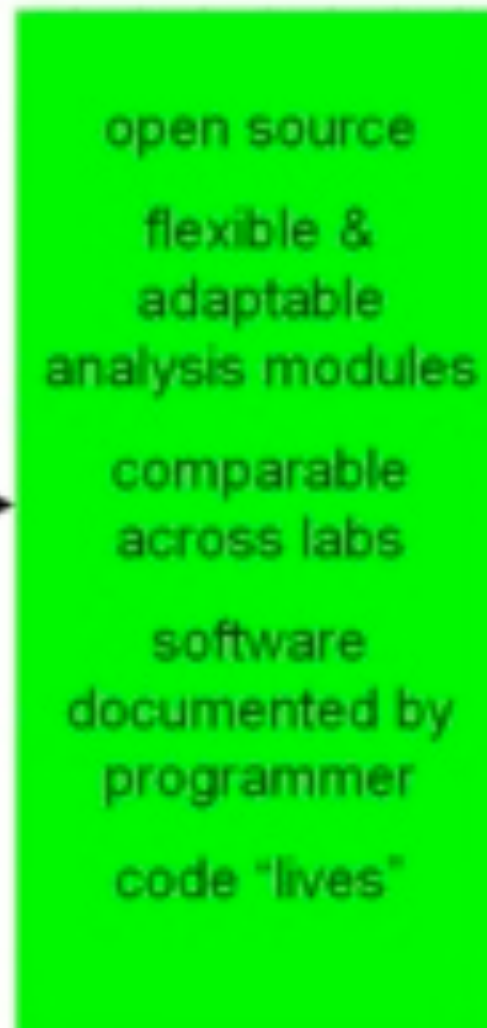


Data Acquisition and Generation



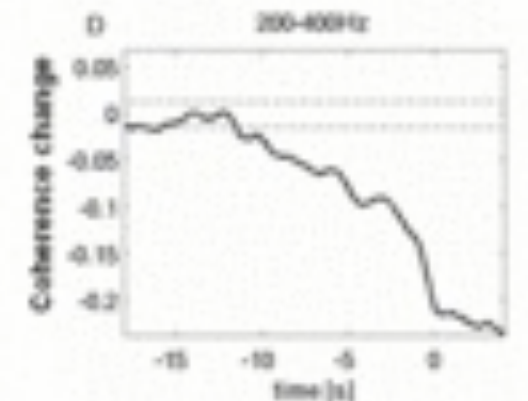
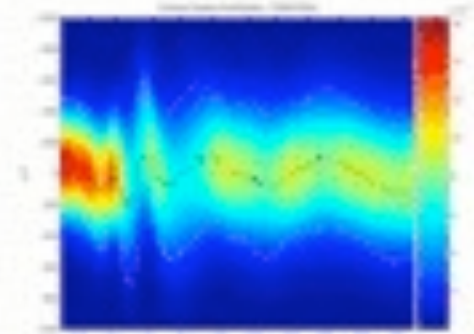
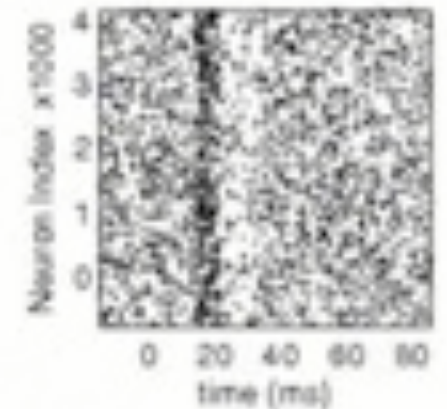
NeuroShare

Analysis Tools

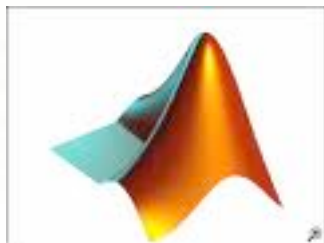


FIND Toolbox

Results



Ralph Meier, BCCN Freiburg



<http://find.bccn.uni-freiburg.de>



<http://neuralensemble.org/NeuroTools>



- **signals**: manipulation of and calculations with spike trains and analog signals.
- **parameters**: management of large, hierarchical parameter sets
- **analysis**: miscellaneous analysis functions
- **stgen**: various stochastic process generators relevant for Neuroscience (Ornstein-Uhlenbeck, Poisson, inhomogenous gamma, ...).
- **plotting**: tools for plotting and image processing, based on Matplotlib and the Python Imaging Library.
- **datastore**: intelligent caching of intermediate results

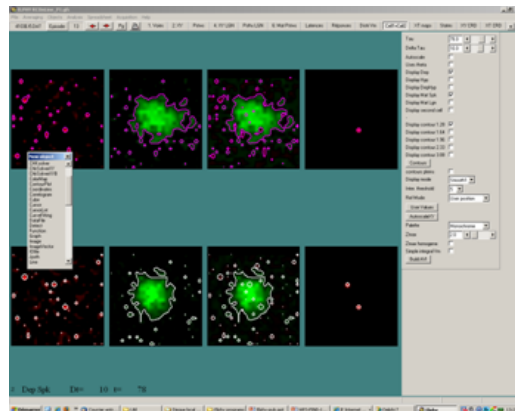
Elphy

- Programmable data acquisition and analysis environment for Windows
- Used for a large fraction of biological experiments within FACETS

Object Oriented Programming

User Friendly Graphic Interface

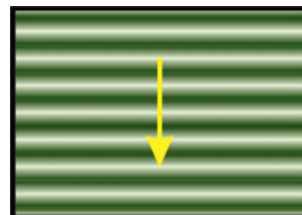
Multi-page display
Owner designed pages
Mouse handling of objects



G. Sadoc
C. Monier
Team: Y. Frégnac

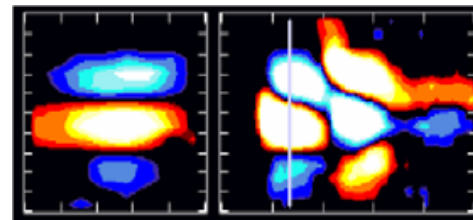
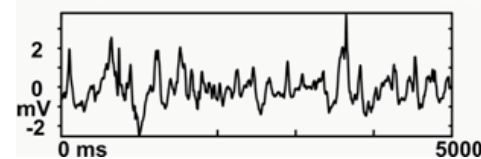
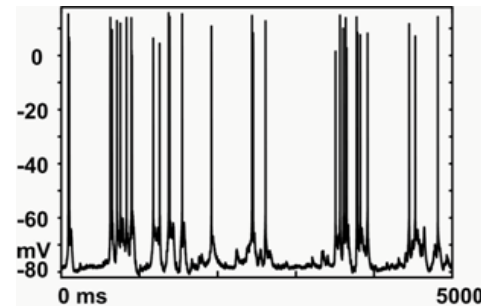
Visual Stimulation

DirectX
Hardware control
Standard graphic adapter



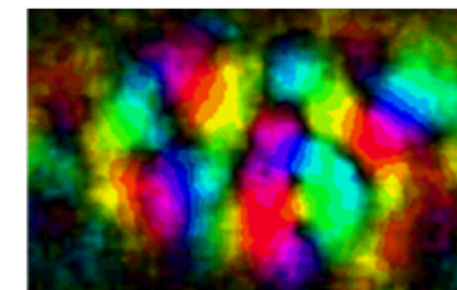
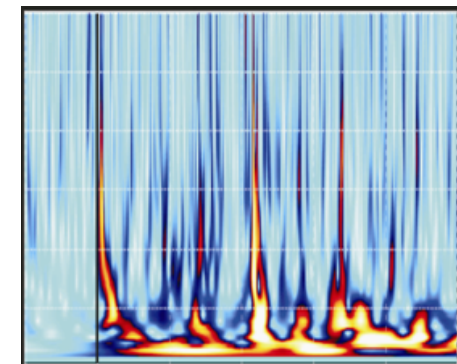
Data Acquisition and Control of Experiments

Interfaces from Axon,
ITC, MCC, UEI
On line analysis



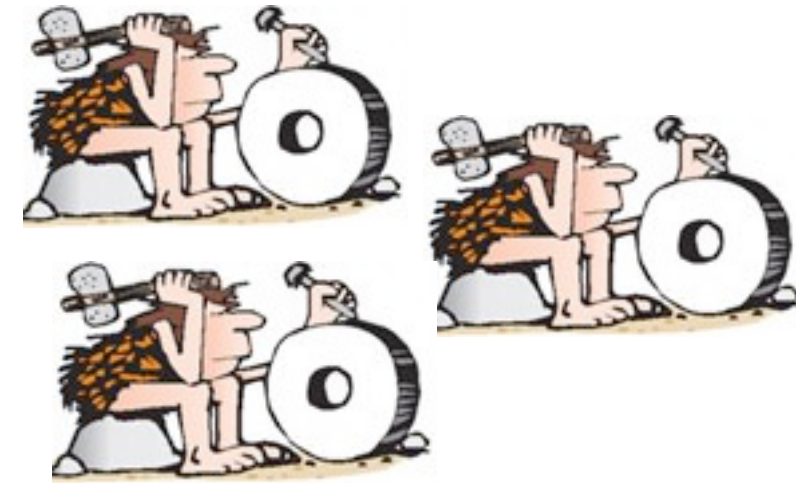
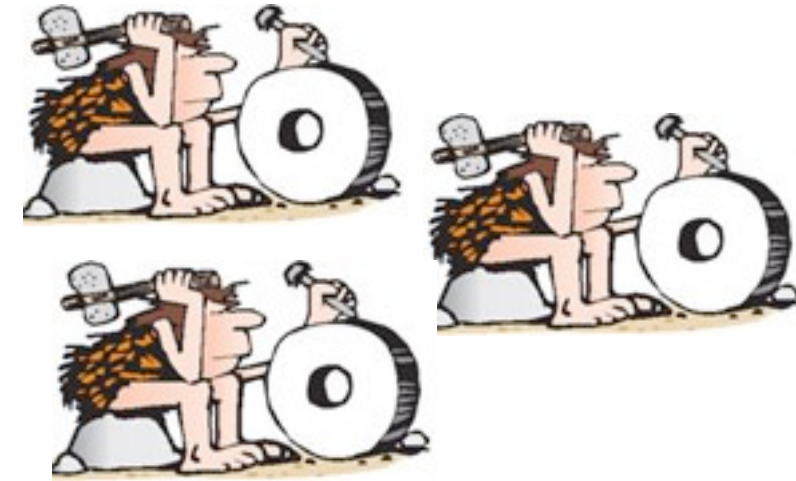
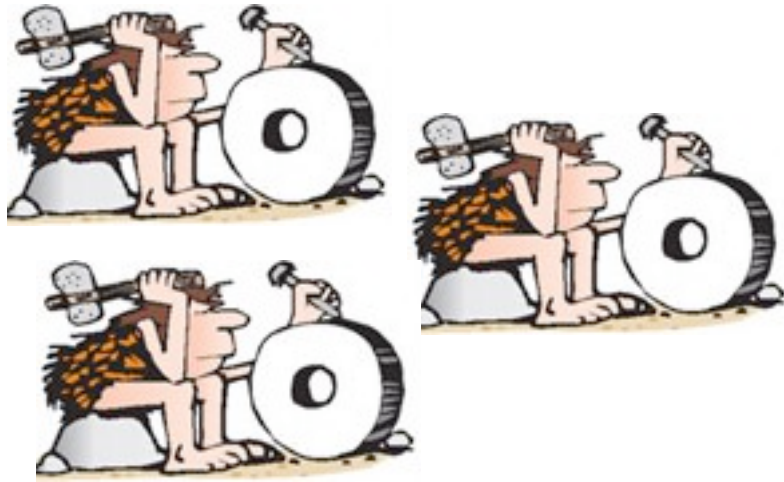
Data Analysis

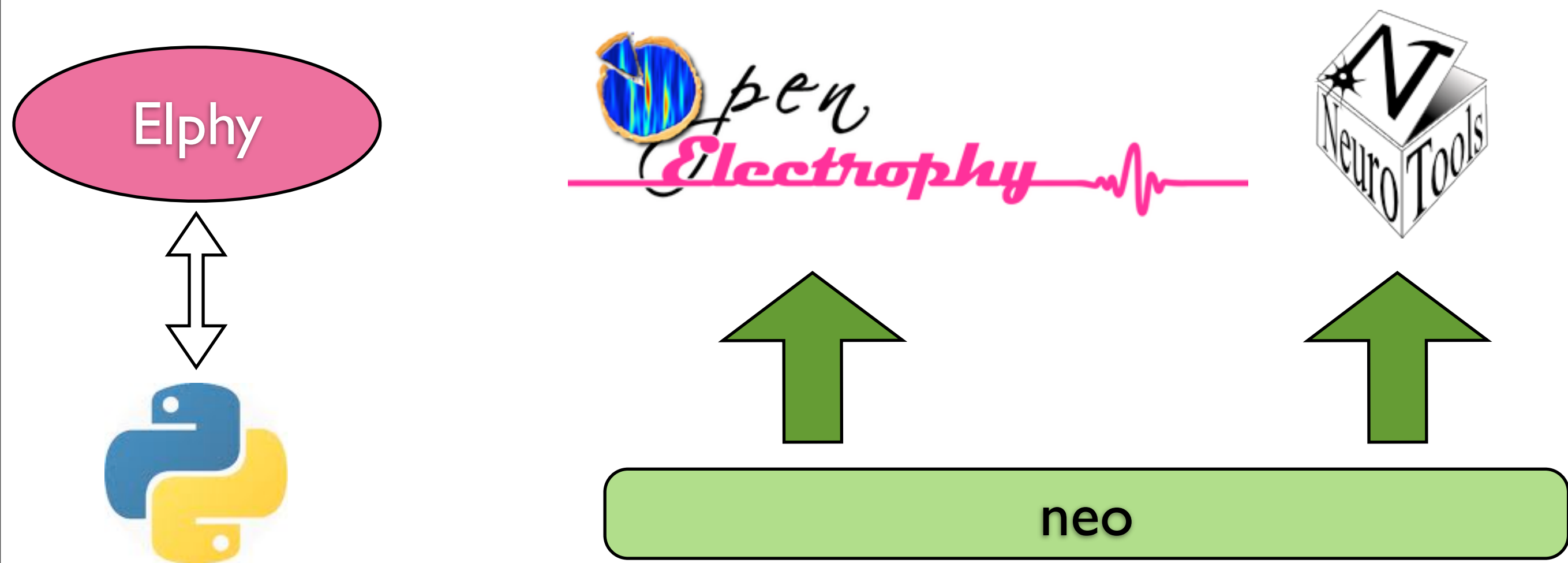
120 dedicated objects
2000 functions
Event detection,
correlations, Fourier
analysis, etc...



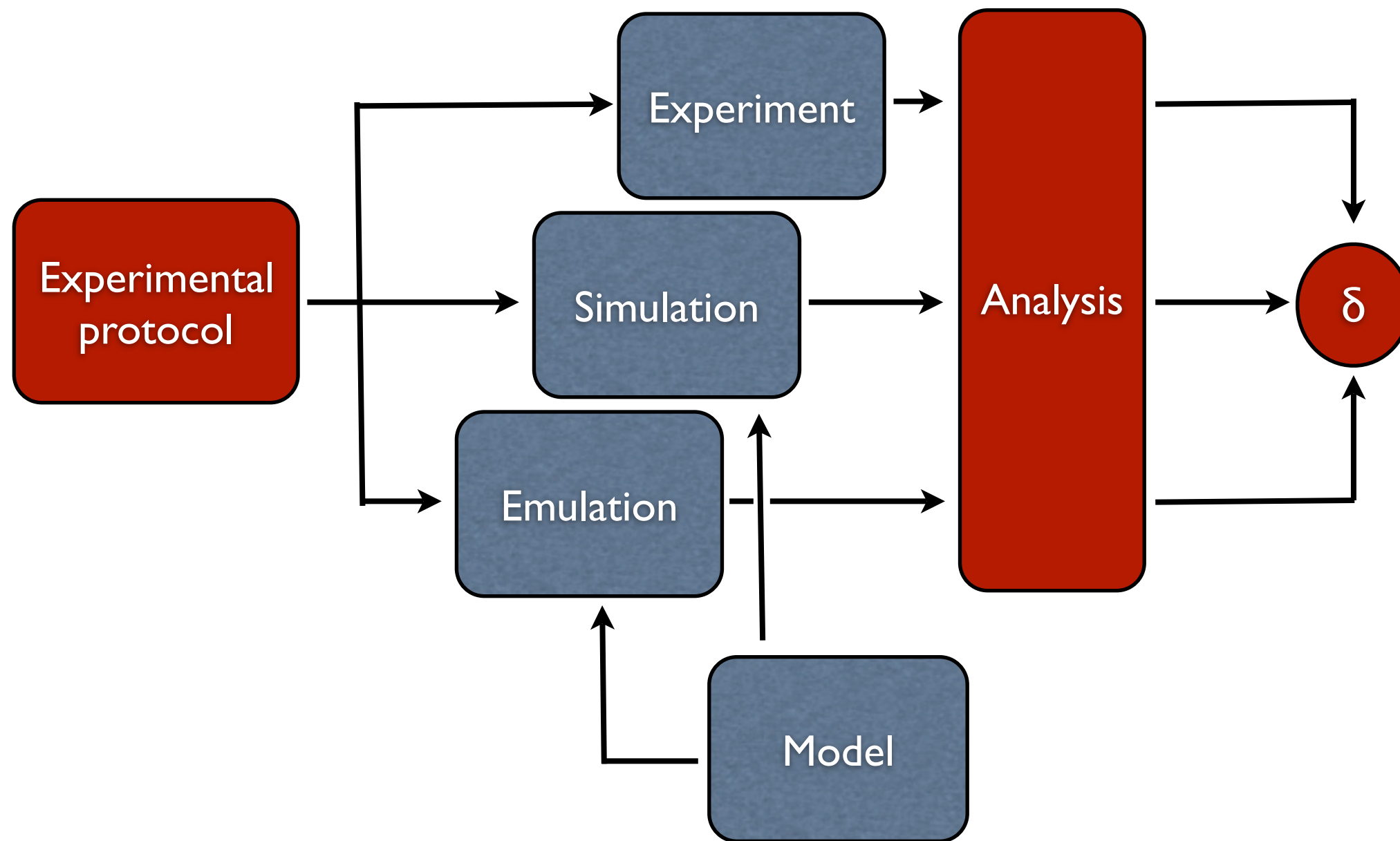
<http://www.unic.cnrs-gif.fr/software.html>

Parallel reimplementation of analysis toolboxes by generations of EC-funded projects?

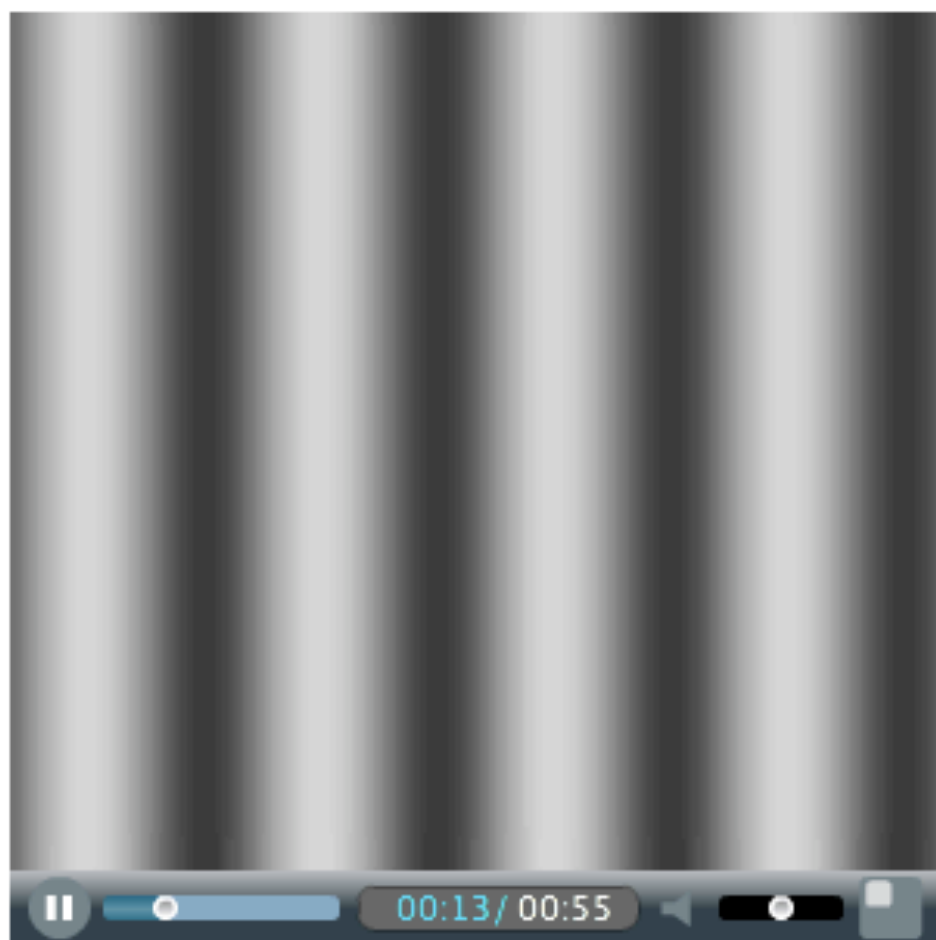




Comparing simulations to experiment



Stimulus *multiple_gratings_20080804-1034.zip* at 94 cd/m²



Reference #	4
Duration (ms)	56000.0
Frame duration (ms)	50.0
Size (pixels)	100,100
Pixels/degree	50.0
Centre (degrees)	3.0,3.0
Max luminance (cd/m ²)	94.0
Background luminance (cd/m ²)	47.0
Variables	contrast, orientation, spatial_freq
Created by	apdavison
Last modified	Fri 12 Dec 2008
Status	public

filter-by-preferred (variable = 'orientation, spatial_freq')



merge trials ()



tuning curve (method = 'mean', variable = 'contrast')



curve fitting (curvetype = 'hyperbolic ratio', method = 'Levenberg-Marquardt', normalization = 'subtract background')



extract parameter (name = 'n')



histogram (binwidth = 0.3, maximum = 7.95, minimum = 0.15)

Encode Materials and Methods in a machine-readable format

6936 • The Journal of Neuroscience, July 30, 2003 • 23(17):6936–6945

Behavioral/Systems/Cognitive

Response to Contrast of Electrophysiologically Defined Cell Classes in Primary Visual Cortex

Diego Contreras and Larry Palmer

Department of Neuroscience, University of Pennsylvania School of Medicine, Philadelphia, Pennsylvania 19106

Information processing in the visual cortex is critically dependent on the input–output relationships of its component neurons. The transformation of synaptic inputs into spike trains depends in turn on the host of intrinsic membrane properties expressed by neurons, which define established electrophysiological cell classes in the neocortex. Here we studied, with intracellular recordings *in vivo*, how the electrophysiological cell classes in the primary visual cortex transform an increasing input, represented by stimulus contrast, into membrane depolarization and trains of action potentials. We used contrast as input because, regardless of their stimulus selectivity, primary visual cortical cells increase their firing rates in response to increases in luminance contrast. We found that both the spike rate response and the membrane potential response are best described by the hyperbolic ratio function when compared with linear, power, and logarithmic functions. In addition, both responses show similar parameter values and similar residual variance from the fits to all four functions. We also found that changes in membrane potential are similar, but firing rates differ strongly, between the established electrophysiological cell classes: fast spiking neurons show the highest firing rates, followed by fast rhythmic bursting, and regular spiking (RS) cells. In addition, among complex cells, RS cells from supragranular layers fired at higher rates than RS cells from infragranular layers. Finally, we show that the differences in firing rates between cell classes arise from differences in the slope of the relationship between membrane potential and spike rate.

Key words: contrast; visual cortex; intrinsic properties; intracellular; *in vivo*; simple; complex

Introduction

A critical step in understanding the operations of local cortical networks is to determine the input–output relationships of its com-

are generally GABAergic inhibitory interneurons, whereas regular spiking (RS) cells are glutamatergic excitatory cells. Therefore, for a functional understanding of cortical operations it is critical

```

<?xml version="1.0" encoding="utf-8"?>
<benchmark id="CoPa03_Fig6A" version="n/a">
  <description>
    Distribution of parameters for hyperbolic ratio function fit to contrast response curves (spike responses). Experimental data from Fig 6A of Contreras and Palmer (2003) J. Neurosci 23: 6936-6945. This is a preliminary version that only finds preferred orientation, not spatial or temporal frequency, only fits the F0 (DC) component of the response, only compares the exponent parameter of the fitted curve to data, and uses full-screen, not localised, drifting gratings.
  </description>
  <recording>
    <measureable>
      spikes
    </measureable>
    <location>
      <brain-region name="V1">
        <layer name="not specified">
          <cell-type name="not specified" number="58"/>
        </layer>
      </brain-region>
    </location>
  </recording>
  <analysis type="filter-by-preferred">
    <parameter name="variable" value="orientation, spatial_freq"/>
  </analysis>
  <analysis type="merge trials"/>
  <analysis type="tuning curve">
    <parameter name="method" value="mean"/>
    <parameter name="variable" value="contrast"/>
  </analysis>
  <analysis type="curve fitting">
    <parameter name="curvetype" value="hyperbolic ratio"/>
    <parameter name="method" value="Levenberg-Marquardt"/>
    <parameter name="normalization" value="subtract background"/>
  </analysis>
  <analysis type="extract parameter">
    <parameter name="name" value="n"/>
  </analysis>
  <analysis type="histogram">
    <parameter name="binwidth" units="" value="0.3"/>
    <parameter name="maximum" units="" value="7.95"/>
    <parameter name="minimum" units="" value="0.15"/>
  </analysis>
  <difference-measure type="χ²"/>
  <protocol duration="56000.0" id="multiple_grating2" repetitions="8" weight="1.0">
    <stimulus background-luminance="47.0" img="https://www.dbunic.cnrs-gif.fr/media/stimuli/multiple_gratings_20080804-1034.zip" max-luminance="94.0" scale-factor="50.0" variables="contrast, orientation, spatial_freq"/>
    <comparison-data url="https://www.dbunic.cnrs-gif.fr/media/fkb/Benchmarks/CoPa03_fig6A_spikes_exponent.dat"/>
  </protocol>
</benchmark>

```

This shows our prototype XML format for describing experiments in a machine-readable format, such that the experiments can be automatically applied to different models...

But who wants to write XML?

The screenshot shows a web browser window with the URL https://www.dbunic.cnrs-gif.fr/benchmark_library/benchmarks/CoPa03_Fig6A/. The page title is "FACETS Vision Benchmarks: CoPa03_Fig6A". The website header includes the FACETS logo and the text "Fast Analog Computing with Emergent Transient States". A navigation menu on the left lists "HOME", "PUBLIC", "INTERNAL", "Visual Benchmark Library", "Benchmarks", "Stimuli", "Analysis workflows", "FKB browser", and "CONTACT". The user is logged in as "apdavisson" with a "Logout" link. The main content area features a "Beta" badge and the title "Visual Benchmark Library Benchmark 'CoPa03_Fig6A'". Below the title is a table of benchmark details:

Access:	public	
Description:	Distribution of parameters for hyperbolic ratio function fit to contrast response curves (spike responses). Experimental data from Fig 6A of Contreras and Palmer (2003) J. Neurosci 23: 6936-6945. This is a preliminary version that only finds preferred orientation, not spatial or temporal frequency, only fits the F0 (DC) component of the response, only compares the exponent parameter of the fitted curve to data, and uses full-screen, not localised, drifting gratings.	
Recording information:	What:	spikes
	Brain region:	V1
	Layer:	not specified
	Cell type:	not specified
	Number of cells:	58
Analysis:	<ol style="list-style-type: none">1. filter-by-preferred (variable = 'orientation, spatial_freq')2. merge trials ()3. tuning curve (method = 'mean', variable = 'contrast')4. curve fitting (curvetype = 'hyperbolic ratio', method = 'Levenberg-Marquardt', normalization = 'subtract background')5. extract parameter (name = 'n')6. histogram (binwidth = 0.3, maximum = 7.95, minimum = 0.15)	
Difference measure:	chi_square	
Protocol 1:	ID:	multiple_grating2
	Repetitions:	8
	Duration:	56000.0
	Stimulus:	multiple_gratings_20080804-1034.zip at 94 cd/m2
	Comparison data:	https://www.dbunic.cnrs-gif.fr/media/fkb/Benchmarks/CoPa03_fig6A_spikes_exponent.dat
	Weight:	1.0

Below the table are links for "Edit this benchmark" and "Export as XML". At the bottom, it says "Created by: apdavisson. Last modified: Tue 16 Dec 2008".

If you use Python...

```
python visionbenchmark.py
    spontaneous_firing_rate_dark.xml
    simpleV1.py
```

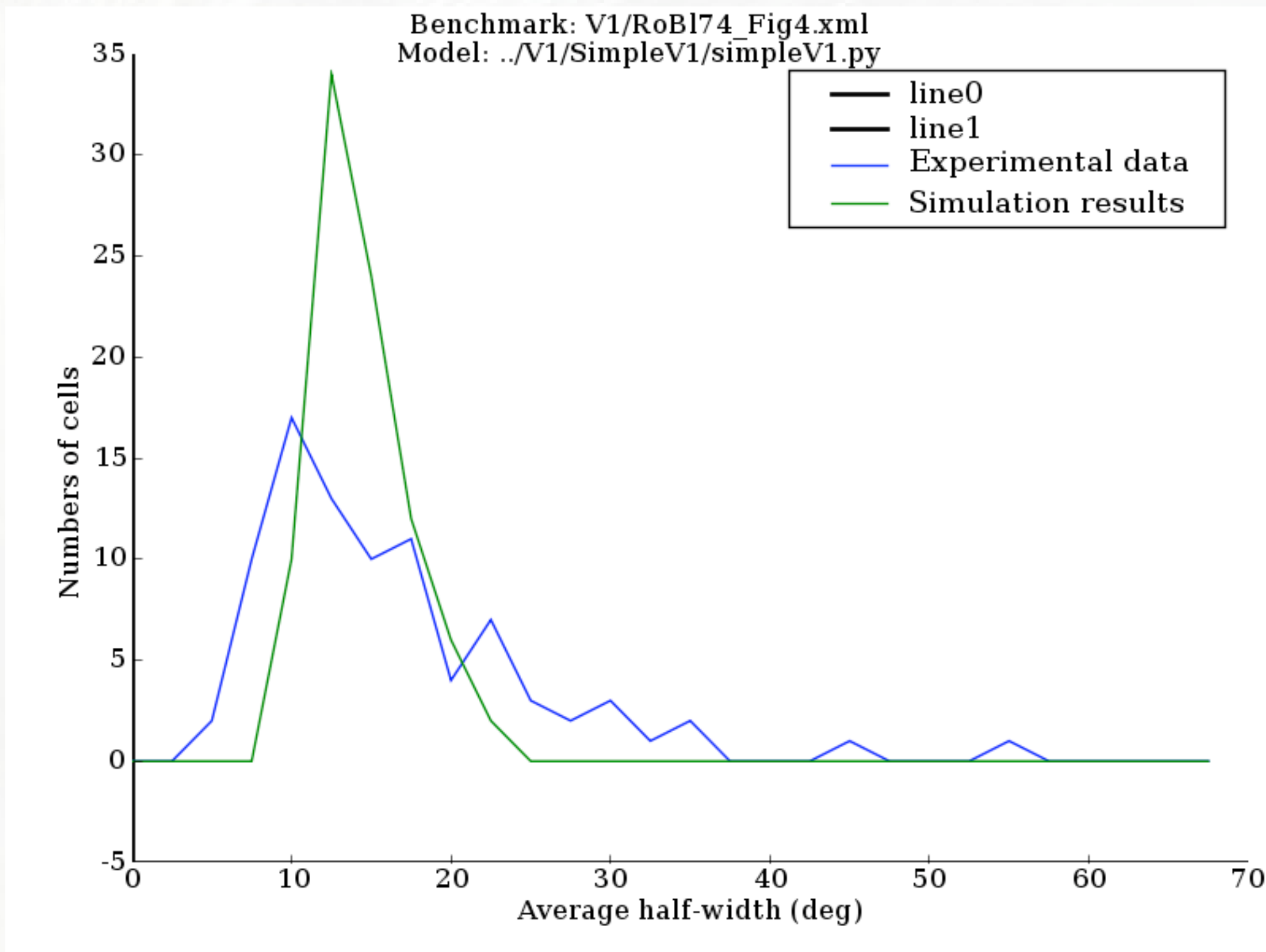
```
Id          spontaneous-firing-rate-dark
Description  Spontaneous firing rate in the dark adapted cat.
Recording.Measureable spikes
Difference_Measure absolute-difference
Analysis 1   mean firing rate

Protocol "dark_screen":
  repetitions:      1
  weight:           1.0
  duration:         10000.0 ms
  scale-factor:     0.1 pixels/degree
  stimulus:         srb://facets.inria.fr/WP5/Benchmarks/VisualStimuli/dark_screen.zip
  max-luminance:   1.0 cd/m2
  comparison-data: 4.0 s-1

Running protocol "dark_screen":


Running retina model .
Analysing results...
  mean firing rate: {'not-specified': (0.0,)}
absolute-difference difference: 4.0
```


Distribution of orientation tuning curve widths



UNIC Helmholtz Database: List of experiments

https://www.dbunic.cnrs-gif.fr/helmholtz/vision/ Google



Home | Vision | Logout | Profile | Help | Contact

List of experiments [Add New Experiment]

Page 1 of 2 ▶

Ref.	Date	Animal	Block recordings
MANIP_2006_18	25/04/2006	Cat, M	6
MANIP_2006_12	22/03/2006	Cat, M	4
MANIP_2006_03	10/01/2006	Cat, FAM130, M	5
MANIP_2006_01	03/01/2006	Cat, ESU173	9
MANIP_2005_49	01/12/2005	Cat, EVP507, M	14
MANIP_2005_05	25/01/2005	Cat, F	2
MANIP_2004_51	13/12/2004		2
MANIP_2004_48	23/11/2004	Cat, EGT721, M	4
MANIP_2004_25	15/06/2004	Cat, DWE772, F, 156 weeks	20
MANIP_2004_22	24/05/2004	Cat, DWE770, F, 156 weeks	4
MANIP_2004_19	04/05/2004	Cat, DVL071, M, 261 weeks	12
MANIP_2004_17	19/04/2004	Cat, DUF306, 365 weeks	5
MANIP_2004_14	30/03/2004	Cat, DVL070, M, 313 weeks	3
MANIP_2004_12	16/03/2004	Cat, F, 108 weeks	6
MANIP_2004_08	17/02/2004	Cat, F	9
MANIP_2004_05	27/01/2004	Cat, 277811, F, 521 weeks	5

In the prototype, we took data from the literature, but of course we would like to make more in-depth comparisons, and, as Wulfram Gerstner said in his talk, if you're going to compare models you need a training set and a testing set, so we would also like to compare to experimental recordings directly. To do this, and to promote the reuse of existing biological data more widely, we've started to develop a database of experimental data obtained during FACETS and previously, from several experimental labs.



Experiment MANIP_2004_25

[\[Edit\]](#) - [\[Delete\]](#)

Date	15th June 2004
Setup	
Experimenters	

Animal

Species	Sex	Tattoo	Age	Weight	Eye Correction
Cat	Female	DWE772	157 weeks	3.2 kg	(dioptrcs)
General Notes		Medical Notes		Behaviour	

Drug Injections

No data available

Drug Perfusions

No data available

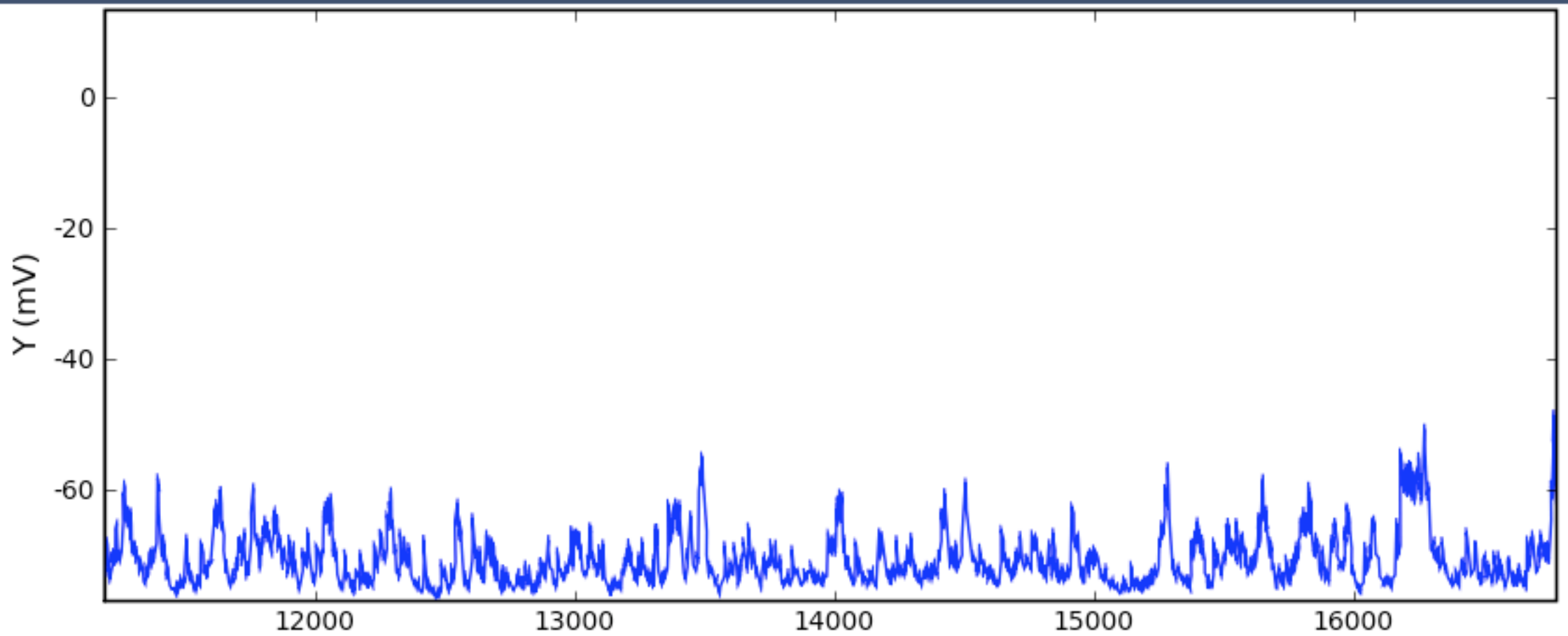
Recording Blocks

Id	Duration (minutes)	Start time	End time	DAT Tapes	Recording method(s)	Elphy Files	Notes
0425A					sharp	0	
0425B					sharp	0	
0425C	45	15-06-2004 04:48	15-06-2004 05:33		sharp	3	
0425D	8	15-06-2004 05:33	15-06-2004 05:41		sharp	0	
0425E	167	15-06-2004 05:41	15-06-2004 08:28		sharp	11	
0425F					sharp	2	
0425G	120	15-06-2004 08:28	15-06-2004 10:28		sharp	9	

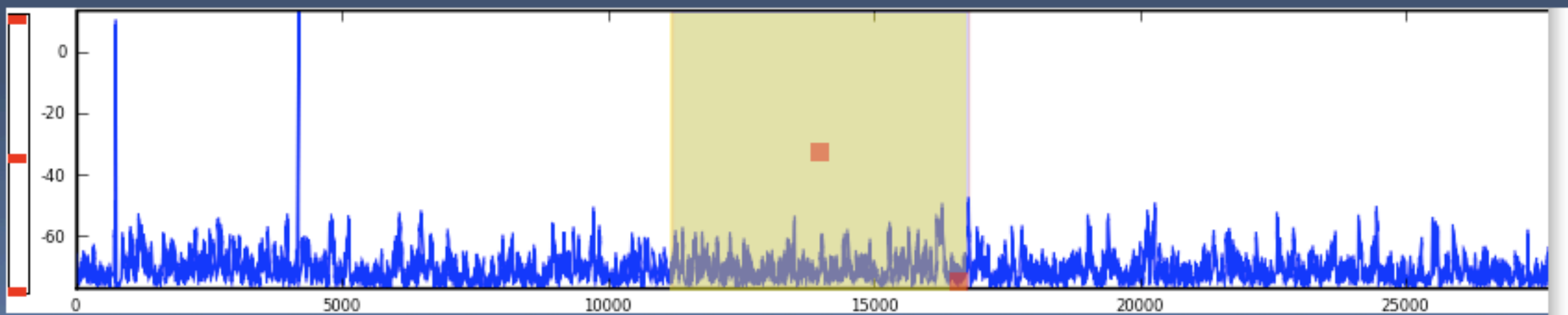
In this database, we aim to capture all the metadata that would be needed either to reproduce an experiment by a biologist, or to reproduce the experiment in a simulation.

This takes time, of course. Here there is data available for the anaesthesia and so forth, but it's all written down in lab notebooks, in bad handwriting, and it takes time to digitize all this stuff.

Zoom



Overview



To improve communication of data and information requires both social change and tool development

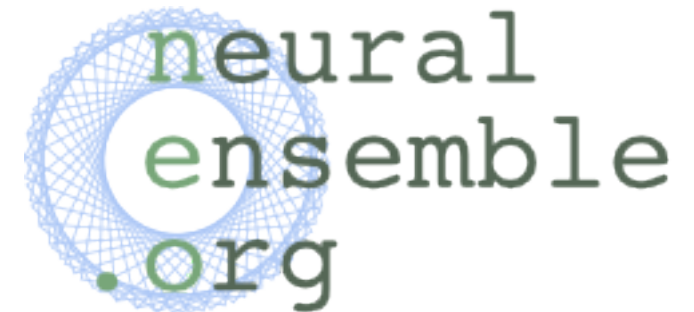
- social/process aspect: **make it normal** to digitize/share data + information
 - carrot: make datasets, etc. citable, count towards career progression
 - stick: funding agencies increasingly require it
- tools aspect: **make it easy** to digitize/share data + information

The best way to get these tools developed is via open collaboration

- large, well-funded, centralized projects
 - (BlueBrain Project, Allen Brain Atlas, ...)
 - have the manpower/resources to develop tools/resolve all these issues internally
- the rest of us
 - can't build all the pieces ourselves
 - need to collaborate, share components
 - either through formal collaborative projects like FACETS, or through informal collaborations
- this is really a false dichotomy
 - large centralised projects often very keen to share what they develop, and benefit from tools developed by others (cf contributions of IBM, etc. to Linux, Google to Python, ...)

Collaborative tool development benefits from formal or informal coordination

- promote discussion
- develop standard interfaces



Acknowledgements

Funding

FET (FACETS)
CNRS



Benchmarking

Jens Kremkow
Klaus Schuch
Mikael Djurfeldt

FIND

Ralph Meier
Christian Garbers
Ulrich Egert



Pierre Yger
Eilif Muller
Daniel Brüderle
Jochen Eppler
Jens Kremkow
Dejan Pecevski

Databases

Thierry Brizzi
Olivier Manette
Cyril Monier
Gérard Sadoc
Zoltan Kisvárdy

Elphy

Gérard Sadoc

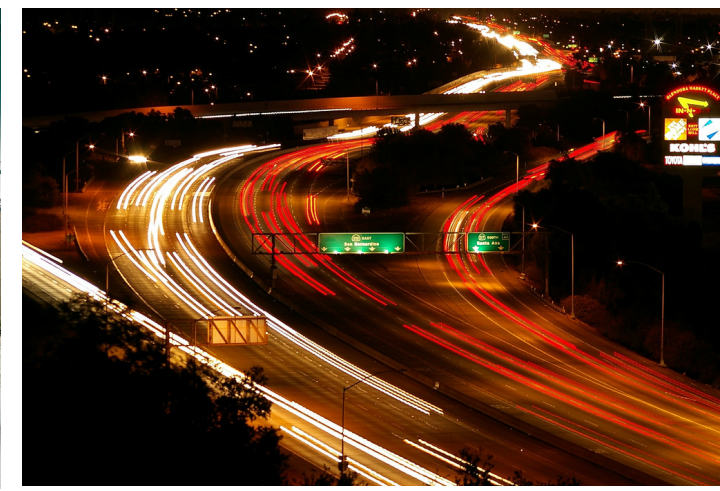


Laurent Perrinet
Pierre Yger
Daniel Brüderle
Eilif Muller
Michael Schmuker
Jens Kremkow
Samuel Garcia
Luc Estebanez

Support and advice

Yves Frégnac
Thierry Viéville
Alain Destexhe
Karlheinz Meier

Conclusions



- the best way to turn the cart-track into the superhighway and help make the complexity of neuromorphic computation manageable is software development in the open
- if you're interested in using and/or helping to develop PyNN, NeuroTools, etc., please check out

<http://neuralensemble.org/>

- if you have a problem, an idea, or are seeking collaborators for your own software project,
 - check out <http://groups.google.com/group/neuralensemble>,
 - or come to the CodeJam <http://neuralensemble.org/codejam4>